

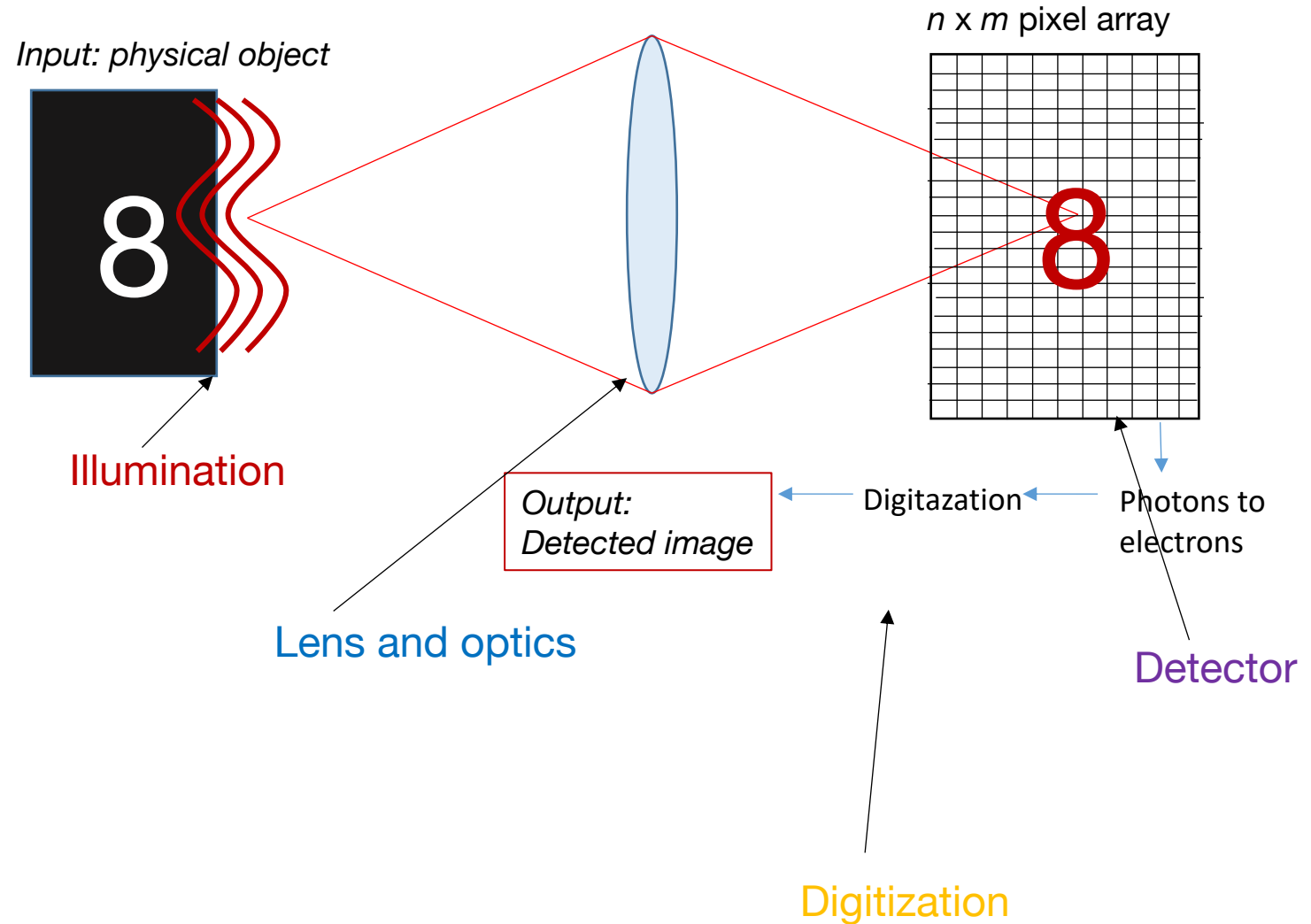
Lecture 19: Physics-based CNN examples

Machine Learning and Imaging

BME 548L
Roarke Horstmeyer

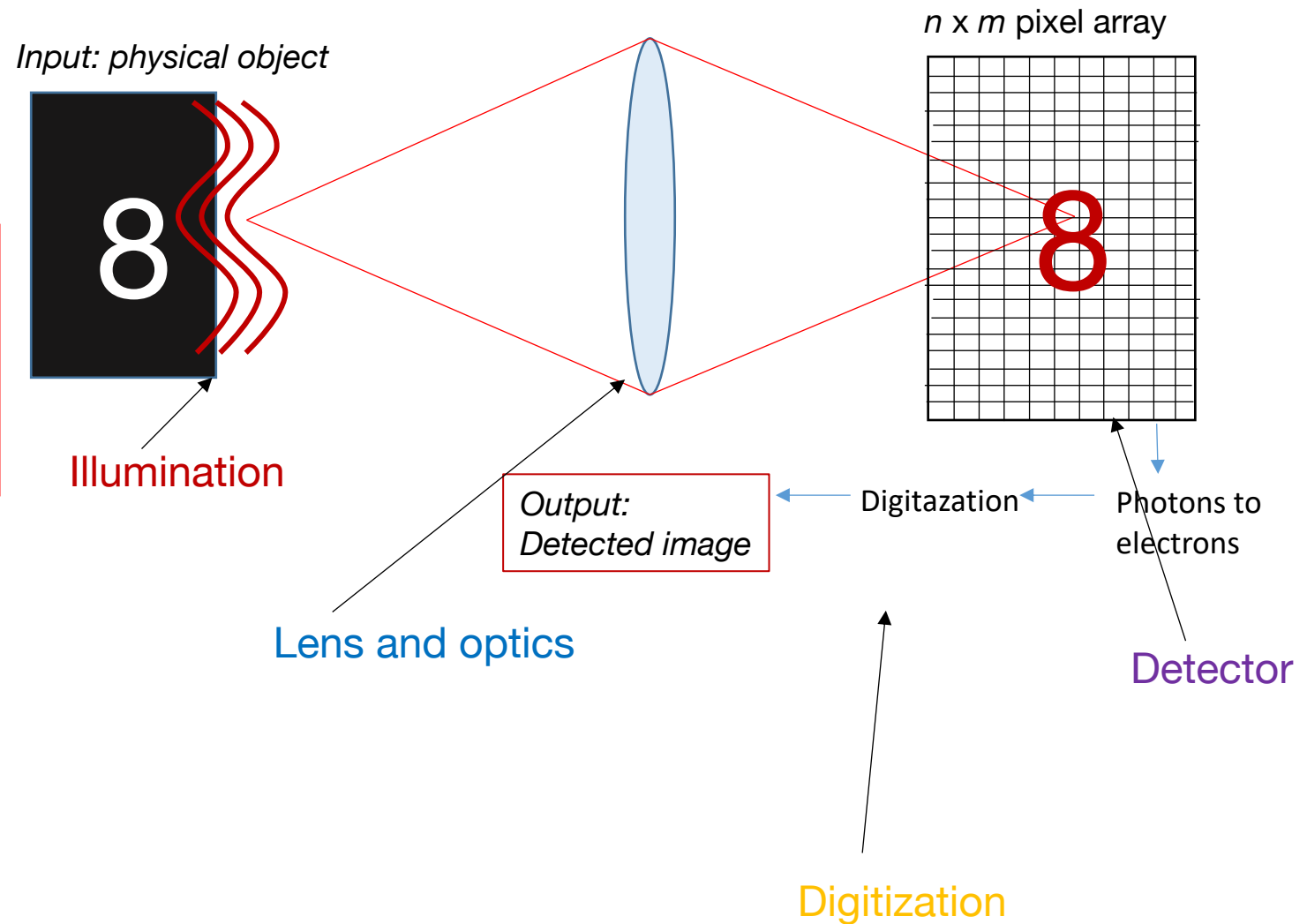
What physical parameters effect image formation?

- **Illumination**
 - Spatial pattern
 - Angle of incidence
 - Color, polarization
- **Lens and optics**
 - Position/orientation
 - Shape
 - Focus
 - Transparency
- **Detector**
 - Pixel size
 - Pixel shape & fill factor
 - Color filters
 - Other filters
- **Digitization**
 - E to P curves
 - Digitization schemes/thresholds
 - Data transmission, multiplexing
- Physical object



What physical parameters effect image formation?

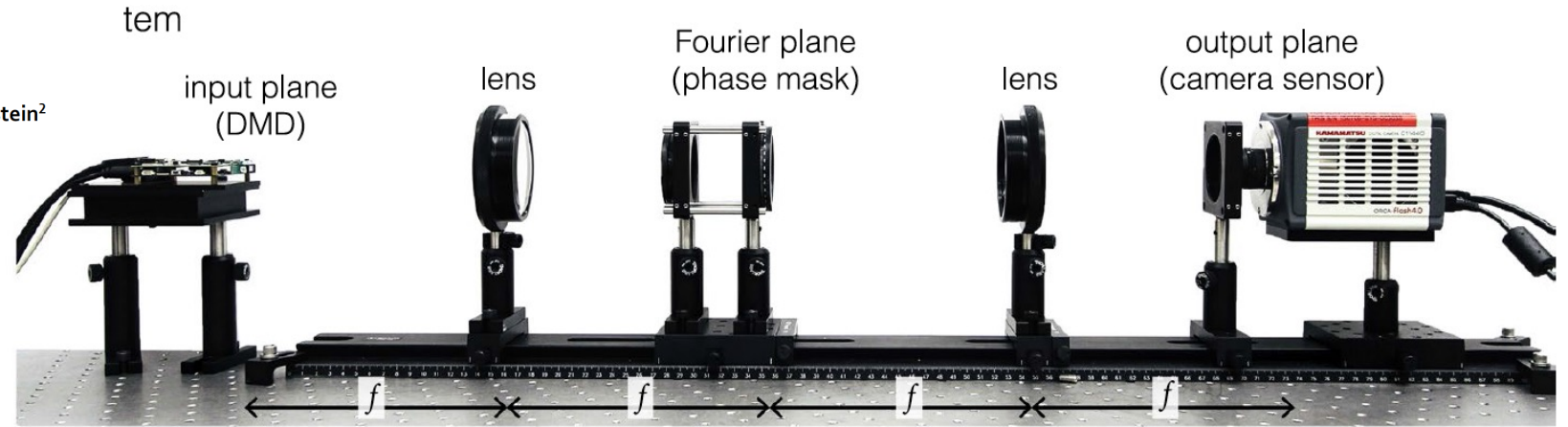
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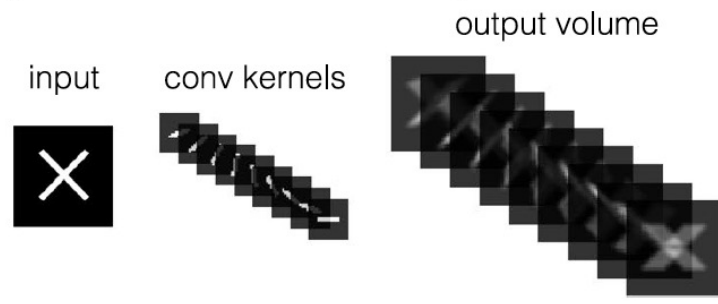
Examples: Lenses and optics

Hybrid optical-electronic convolutional neural networks with optimized diffractive optics for image classification

Julie Chang¹, Vincent Sitzmann², Xiong Dun³, Wolfgang Heidrich³ & Gordon Wetzstein²



b) Standard convolutional layer



c) Optical convolutional layer

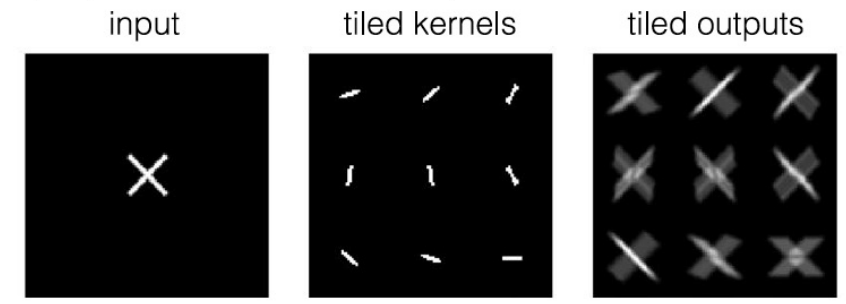
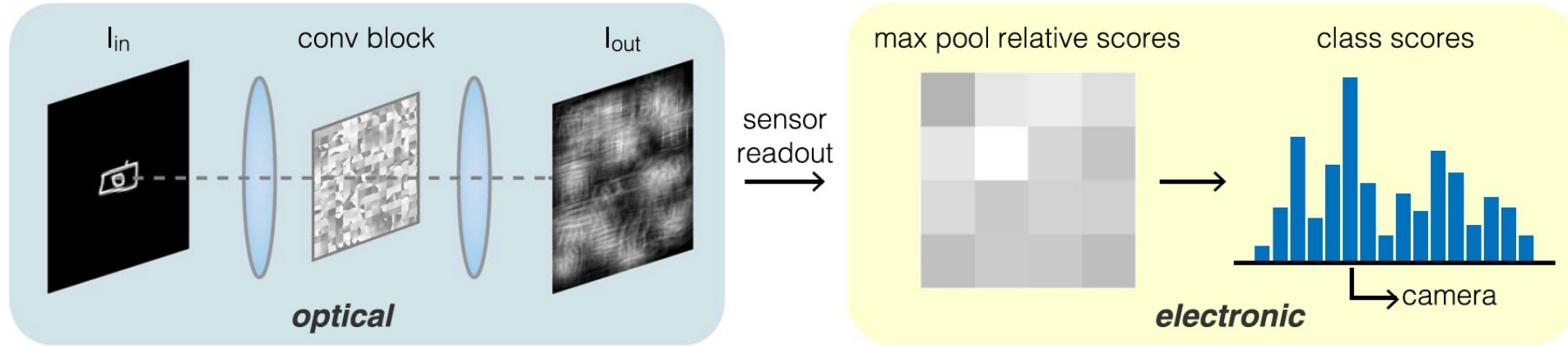


Figure 1. Optical convolutional layer design. (a) Diagram of a $4f$ system that could be adapted to implement optical convolutional (opt-conv) layers by placing a phase mask in the Fourier plane. (b) The standard components of a digital convolutional layer, including an input image, a stack of convolutional kernels, and a corresponding output volume. (c) The equivalent components in an opt-conv layer, where the kernels and outputs are tiled in a 2D array instead of stacked in the depth dimension.

a) Schematic of an optical correlator

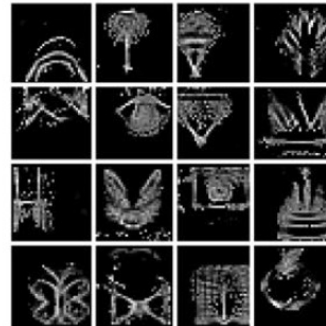


b) Optimized kernels

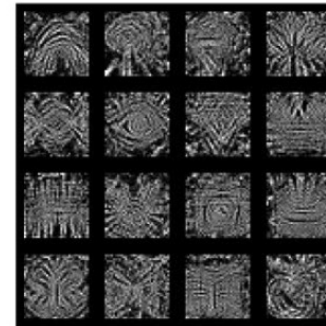
multichannel, unconstrained
accuracy = 0.7591



multichannel, nonneg.
accuracy = 0.7786



tilted kernels, nonneg.
accuracy = 0.7222



optimized phase mask PSF
accuracy = 0.7013

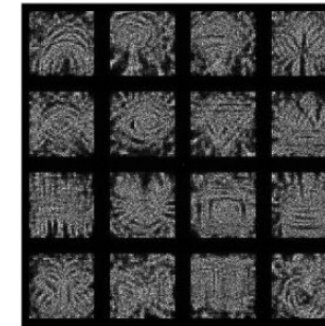


Figure 2. Learned optical correlator. (a) Schematic of an optical correlator, where the conv block consists of the $4f$ system shown in Fig. 1. (b) Characteristic optimized kernels of a multichannel unconstrained digital convolutional layer, a multichannel nonnegative digital convolutional layer, a single channel opt-conv layer with tiled kernels, and the PSF produced by phase mask optimization with the previous optimized tiled kernels as the target.

c) Comparison of simulation and experimental prototype

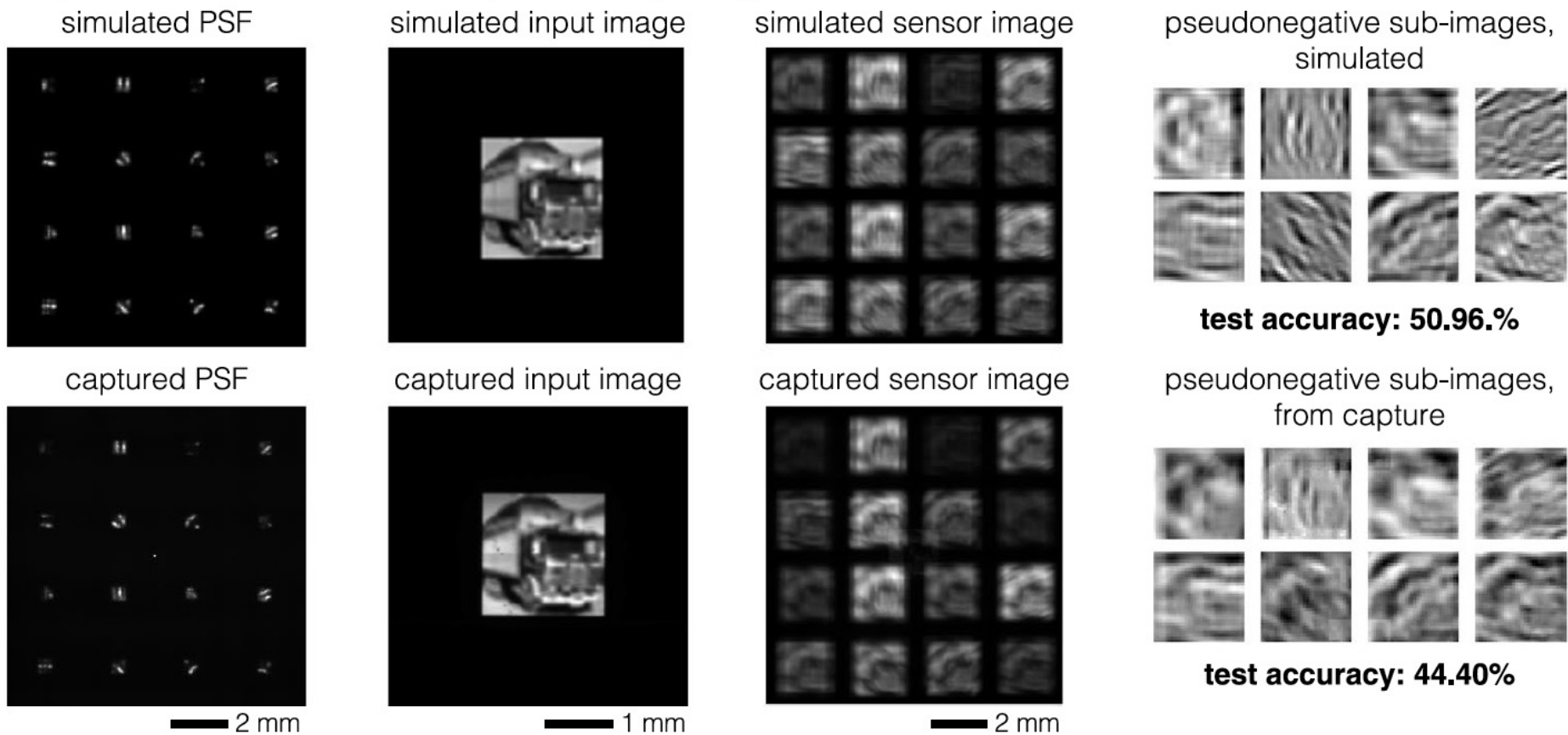


Figure 3. Hybrid optoelectronic CNN. (a) Schematic of a model with a single opt-conv layer, after which the sensor image is processed and fed into subsequent digital CNN layers. (b) The optimized phase mask template and microscope images of the fabricated phase mask, at different zoom levels. (c) Comparison of simulated and captured versions of the PSF produced by the phase mask, a sample input image, the respective sensor image, and pseudonegative sub-images after subtraction of corresponding positive (top two rows) and negative (bottom two rows) sub-images.

End-to-end Optimization of Optics and Image Processing for Achromatic Extended Depth of Field and Super-resolution Imaging

VINCENT SITZMANN*, Stanford University, USA

STEVEN DIAMOND*, Stanford University, USA

YIFAN PENG*, The University of British Columbia, Canada and Stanford University, USA

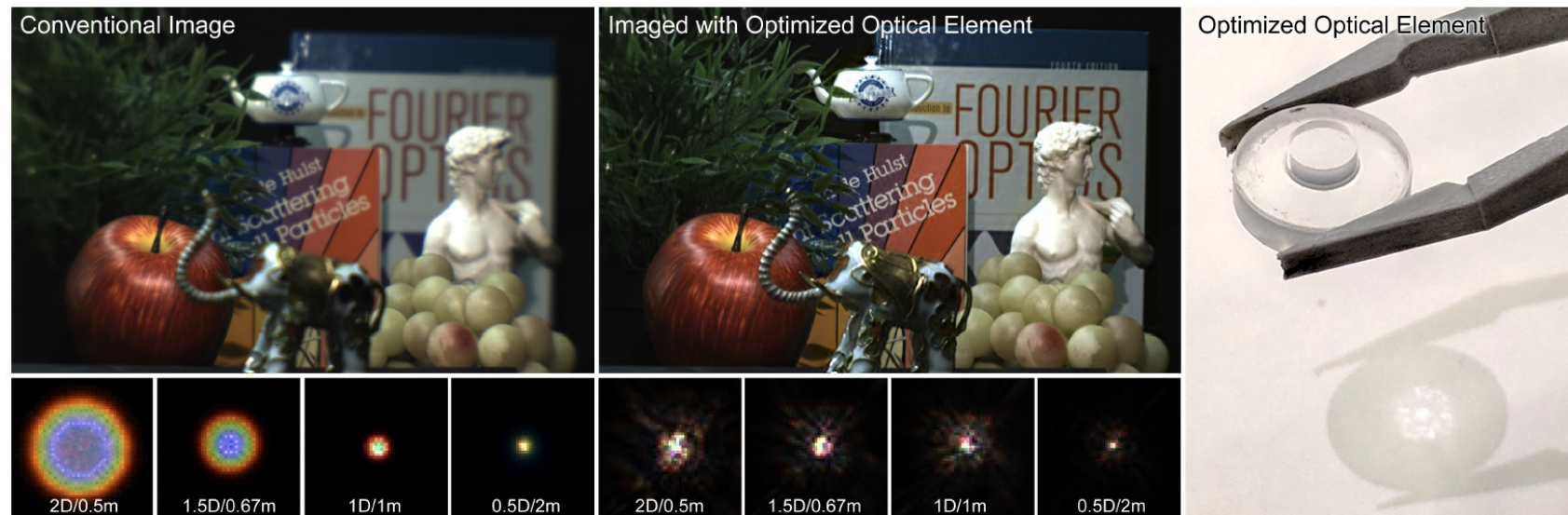
XIONG DUN, King Abdullah University of Science and Technology, Saudi Arabia

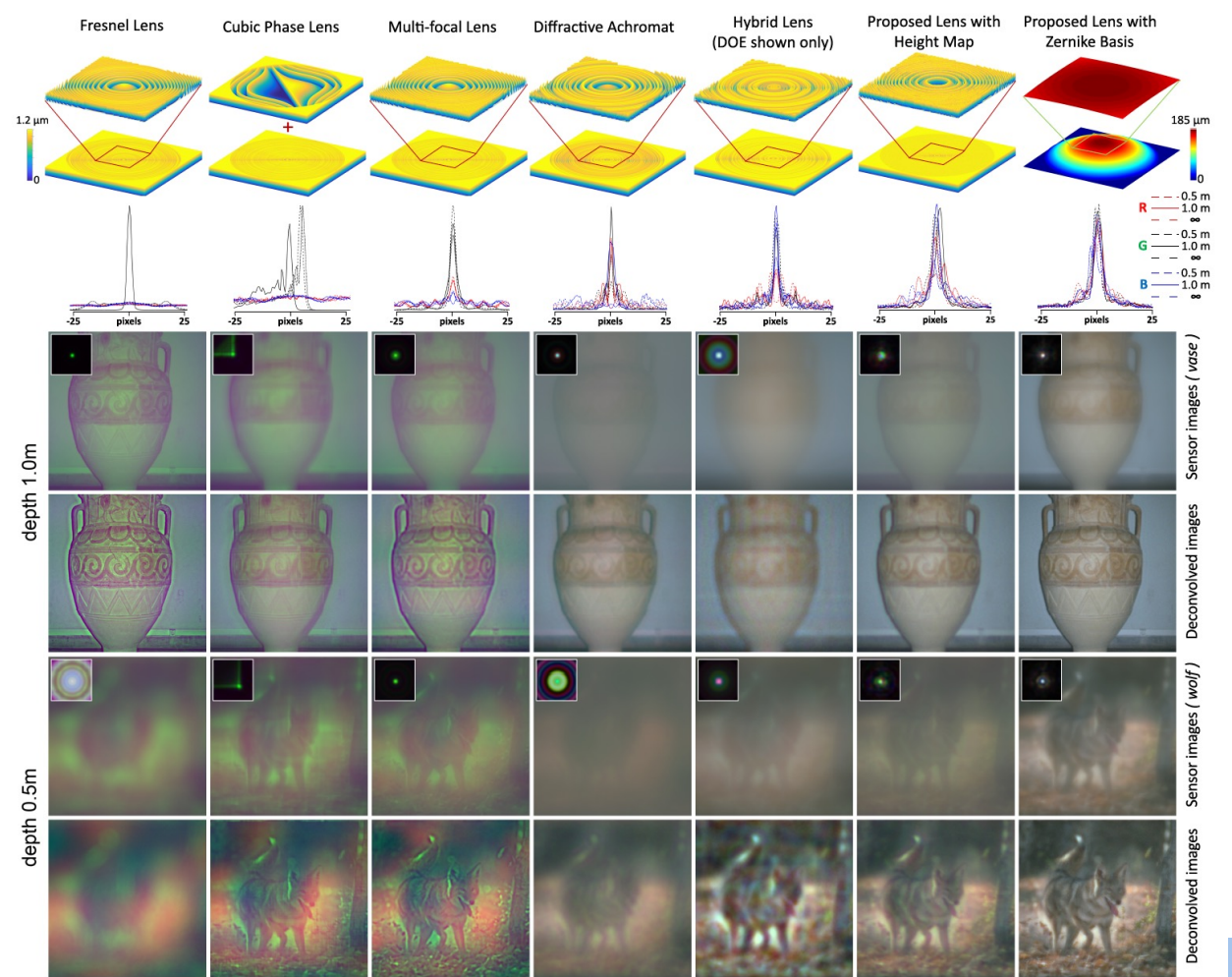
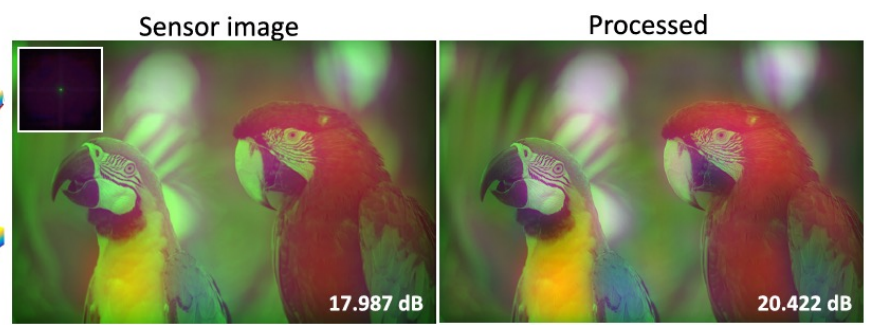
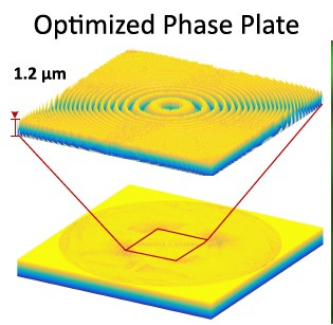
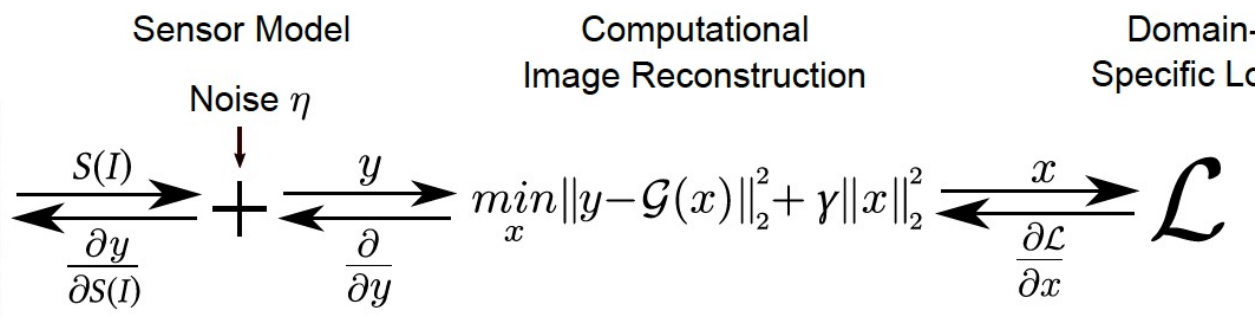
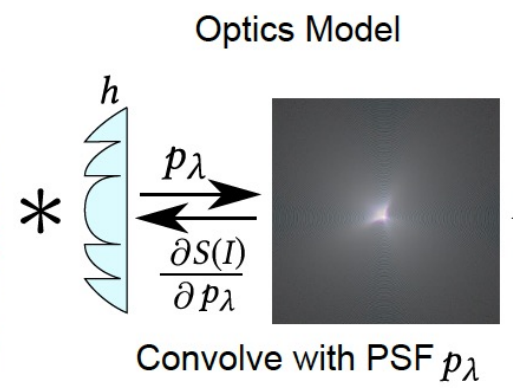
STEPHEN BOYD, Stanford University, USA

WOLFGANG HEIDRICH, King Abdullah University of Science and Technology, Saudi Arabia

FELIX HEIDE, Stanford University, USA

GORDON WETZSTEIN, Stanford University, USA

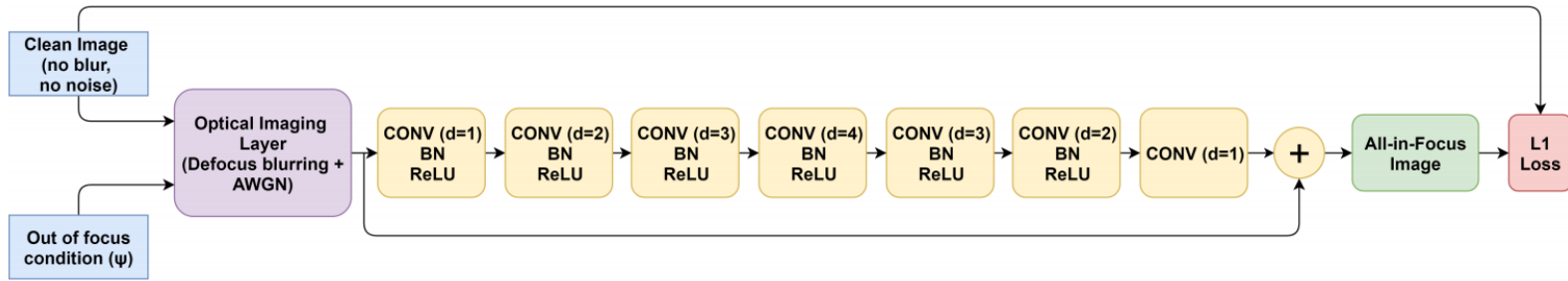
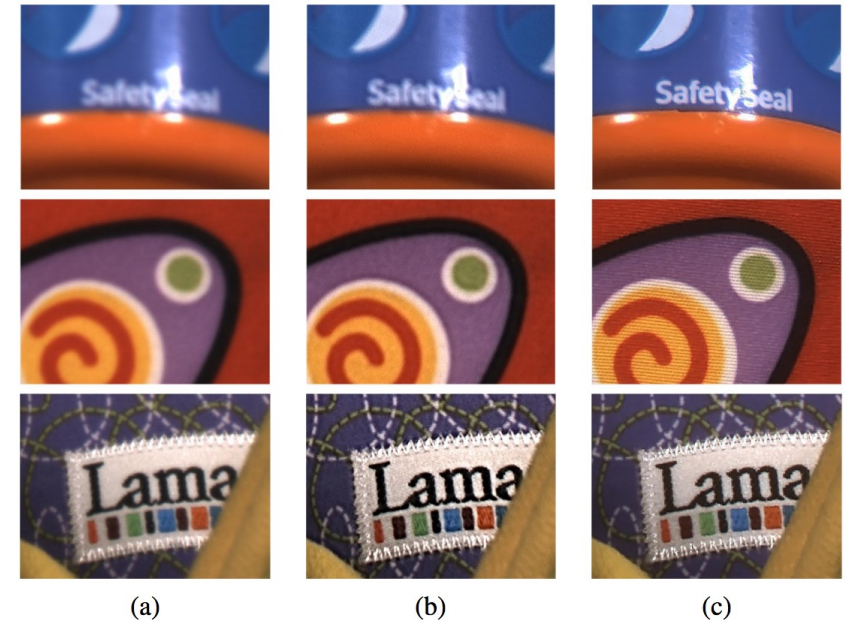
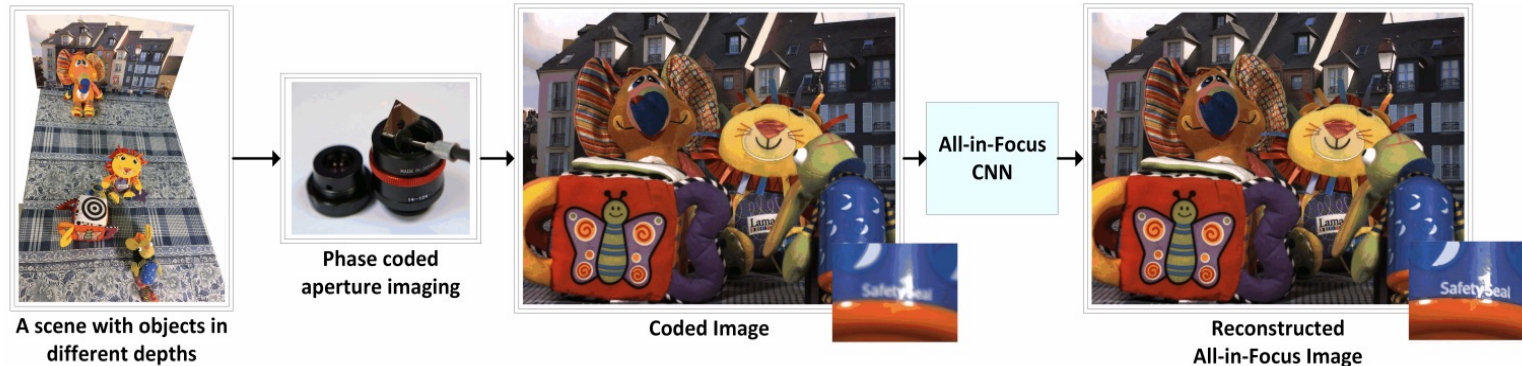




Learned phase coded aperture for the benefit of depth of field extension

SHAY ELMALEM,* RAJA GIRYES, AND EMANUEL MAROM

School of Electrical Engineering, The Iby and Aladar Fleischman Faculty of Engineering, Tel Aviv University, Tel Aviv, Israel
 *shay.elmalem@gmail.com



Multicolor localization microscopy and point-spread-function engineering by deep learning

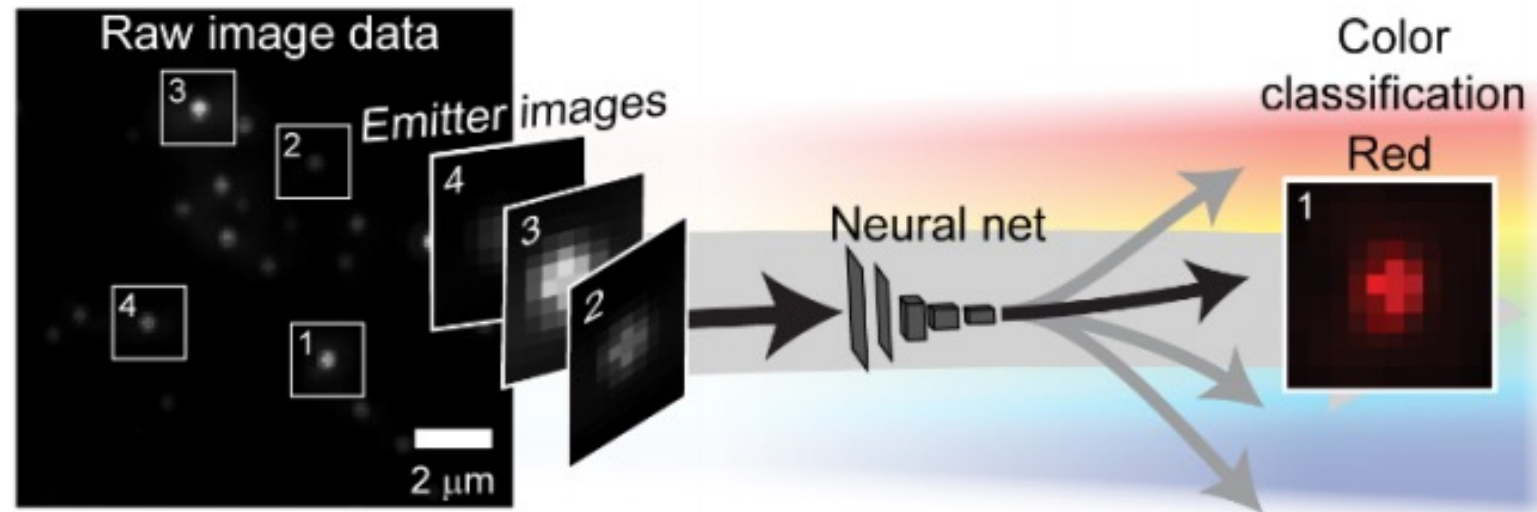
ERAN HERSHKO,^{1,2,3} LUCIEN E. WEISS,^{2,3} TOMER MICHAELI,¹ AND YOAV SHECHTMAN,^{2,*}

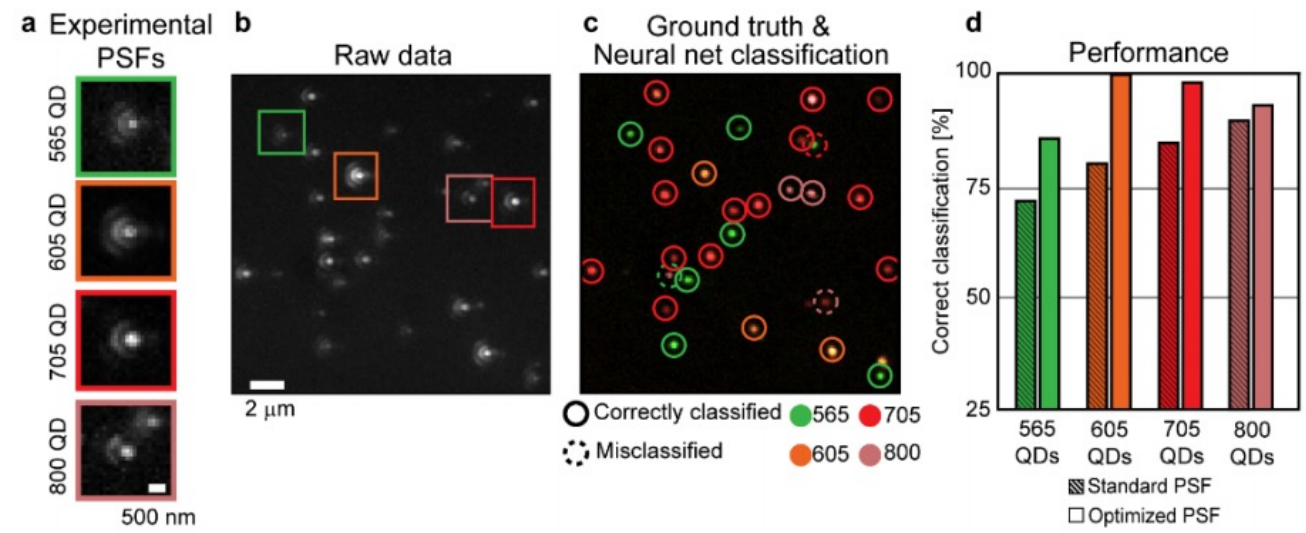
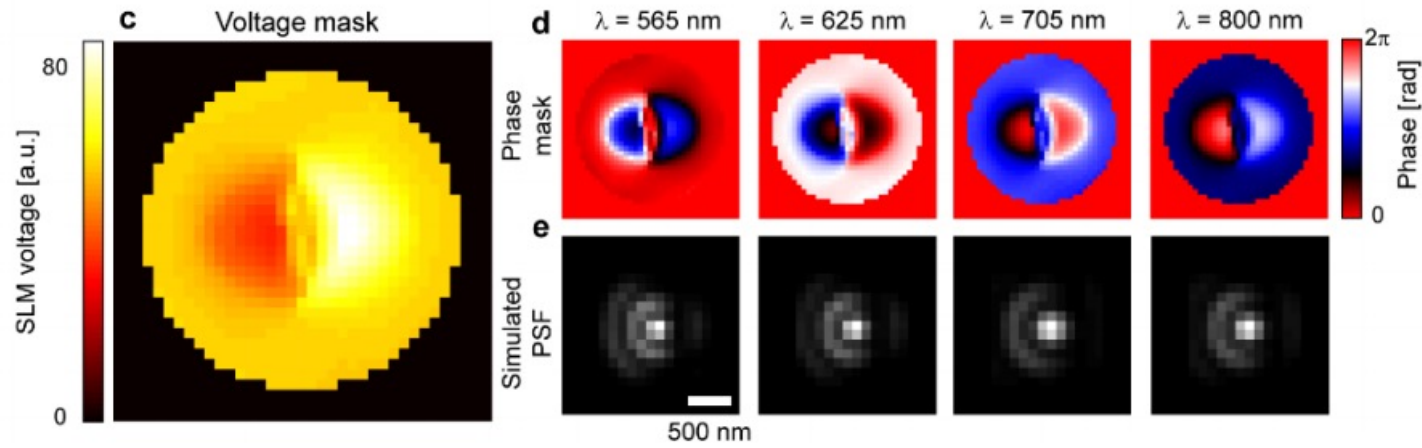
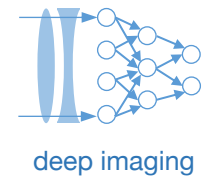
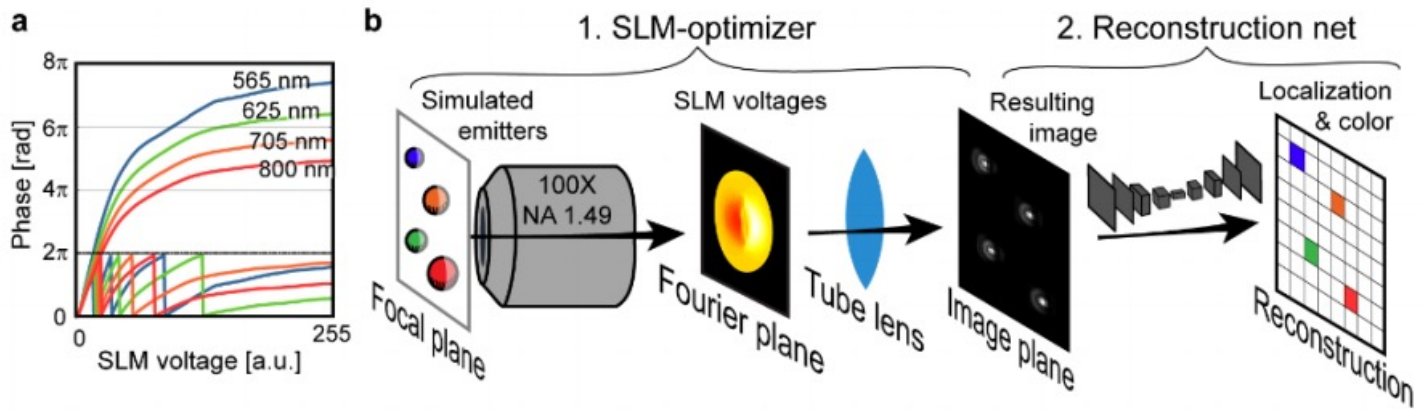
¹*Electrical Engineering Department, Technion, 32000 Haifa, Israel*

²*Biomedical Engineering Department, Technion, 32000 Haifa, Israel*

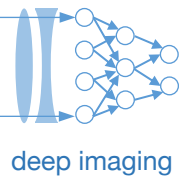
³*Equal contribution*

[*yoavsh@bm.technion.ac.il](mailto:yoavsh@bm.technion.ac.il)

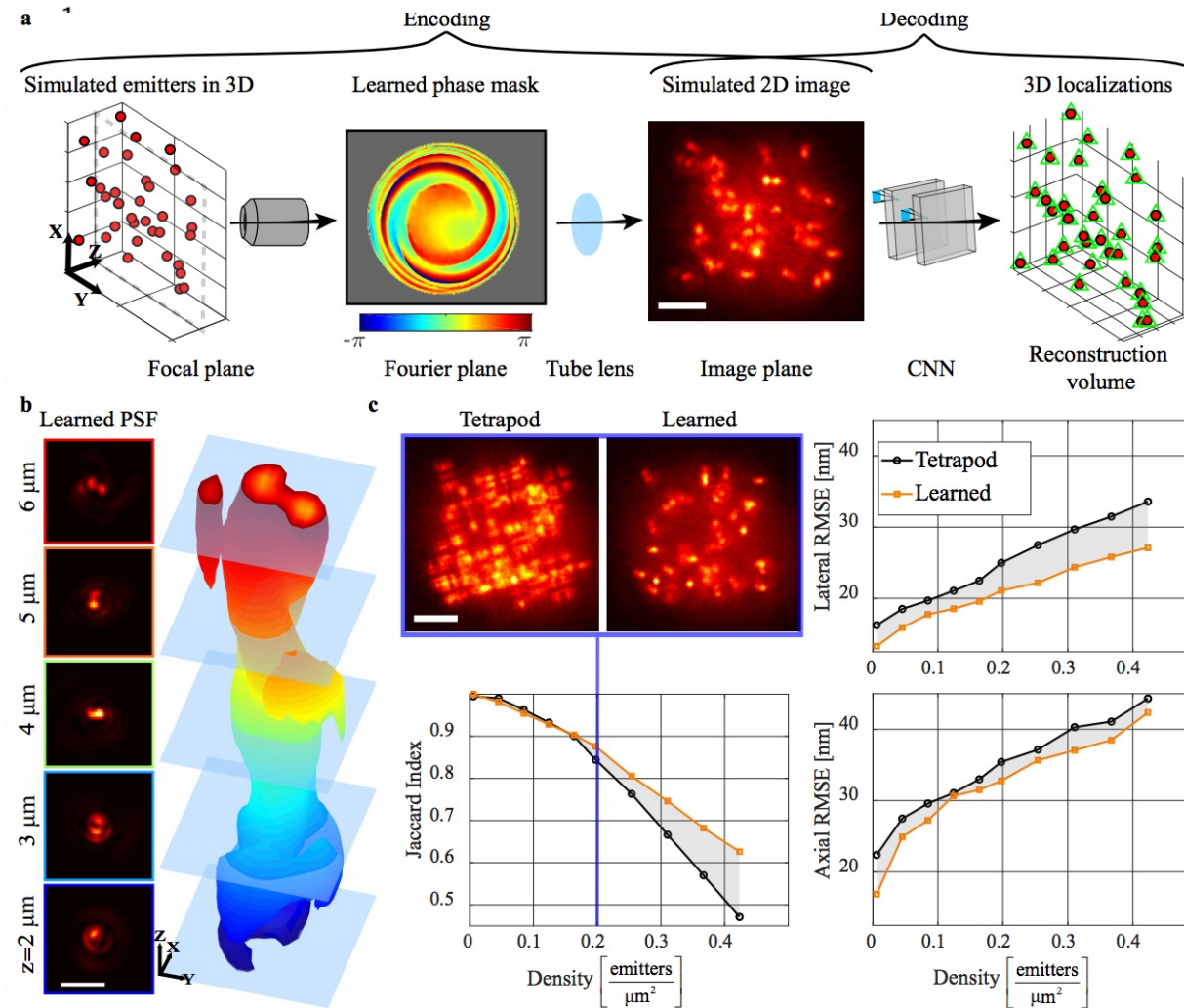




DeepSTORM3D: dense three dimensional localization microscopy and point spread function design by deep learning

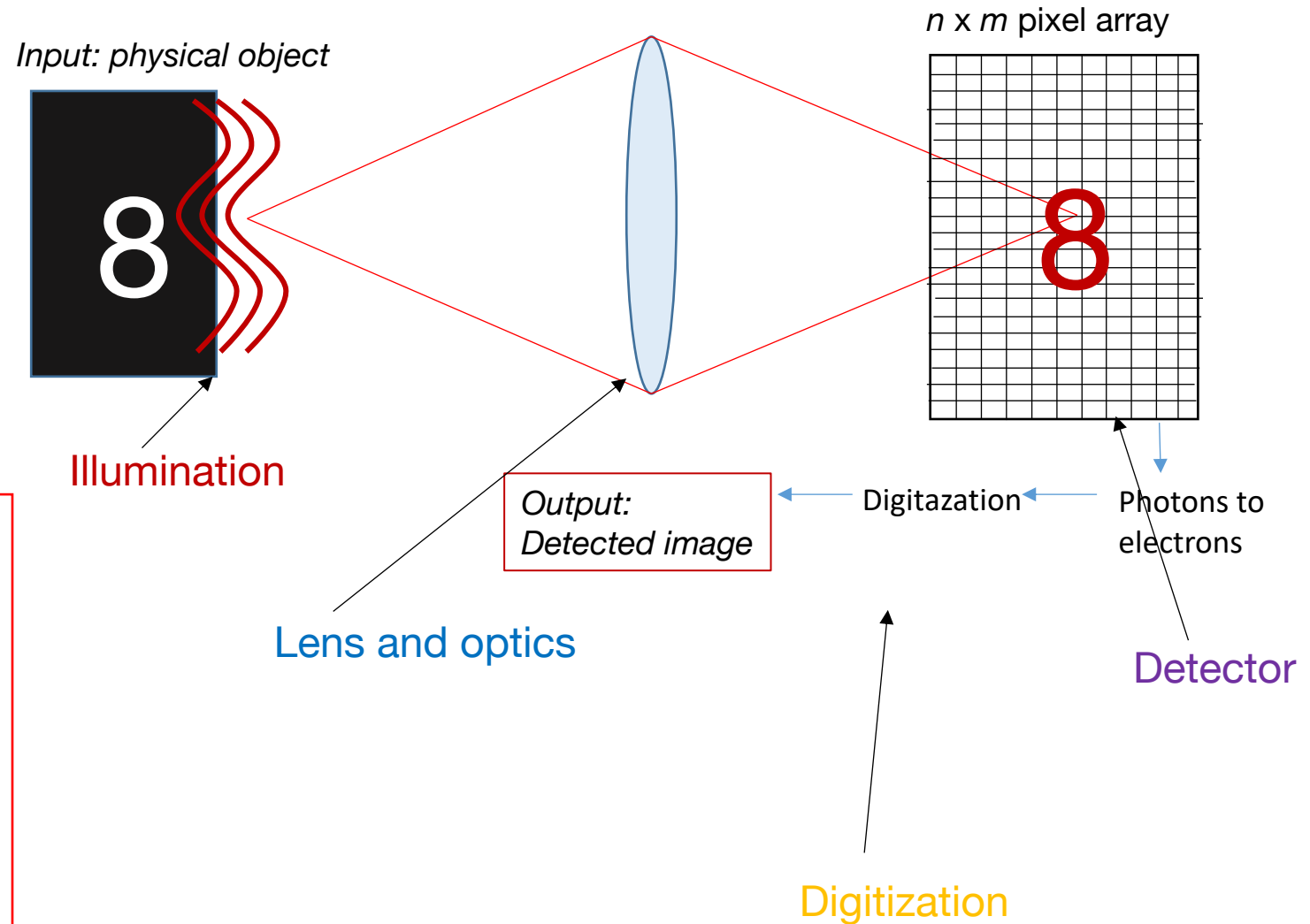


Elias Nehme^{1,2}, Daniel Freedman³, Racheli Gordon², Boris Ferdman^{2,4}, Lucien E. Weiss², Onit Alalouf², Reut Orange^{2,4}, Tomer Michaeli¹, and Yoav Shechtman^{2,4,*}



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Examples: Detection and sampling

DEEP LEARNING SPARSE TERNARY PROJECTIONS FOR COMPRESSED SENSING OF IMAGES

Duc Minh Nguyen, Evaggelia Tsiligianni, Nikos Deligiannis

Vrije Universiteit Brussel, Pleinlaan 2, B-1050 Brussels, Belgium
imec, Kapeldreef 75, B-3001 Leuven, Belgium

Email: {mdnguyen, etsiligi, ndeligia}@etrovub.be

DeepBinaryMask: Learning a Binary Mask for Video Compressive Sensing

Michael Iliadis, *Member, IEEE*, Leonidas Spinoulas, *Member, IEEE*,
and Aggelos K. Katsaggelos, *Fellow, IEEE*

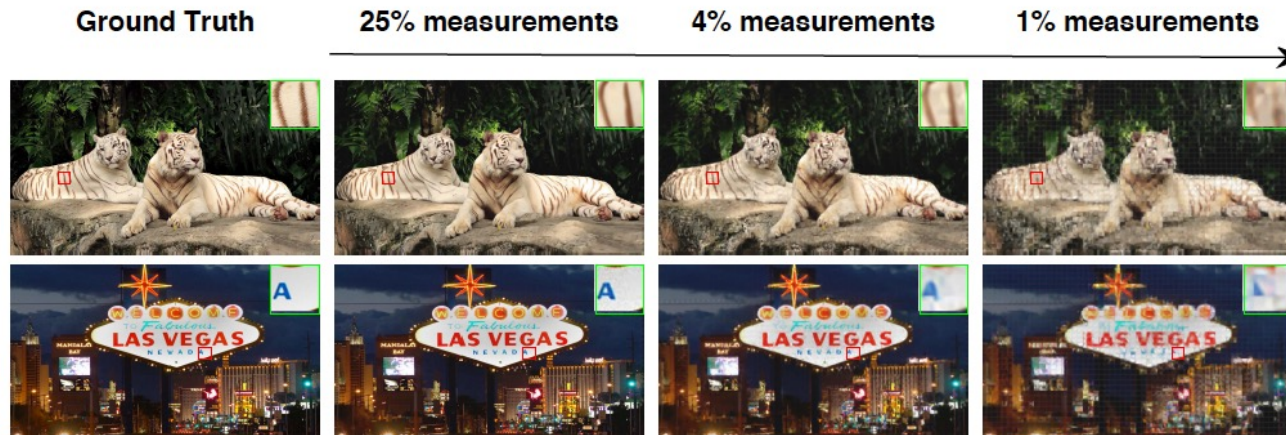
ReconNet: Non-Iterative Reconstruction of Images from Compressively Sensed Random Measurements

Kuldeep Kulkarni^{1,2}, Suhas Lohit¹, Pavan Turaga^{1,2}, Ronan Kerviche³, and Amit Ashok³

¹School of Electrical, Computer, and Energy Engineering, Arizona State University, Tempe, AZ

²School of Arts, Media and Engineering, Arizona State University, Tempe, AZ

³College of Optical Sciences, University of Arizona, Tucson, AZ



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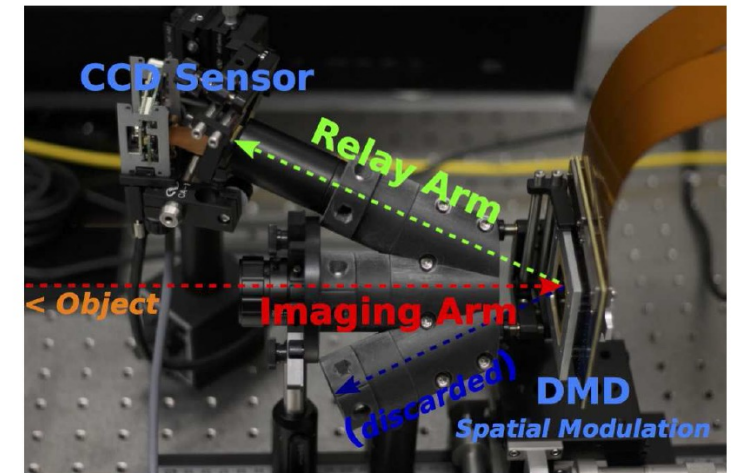
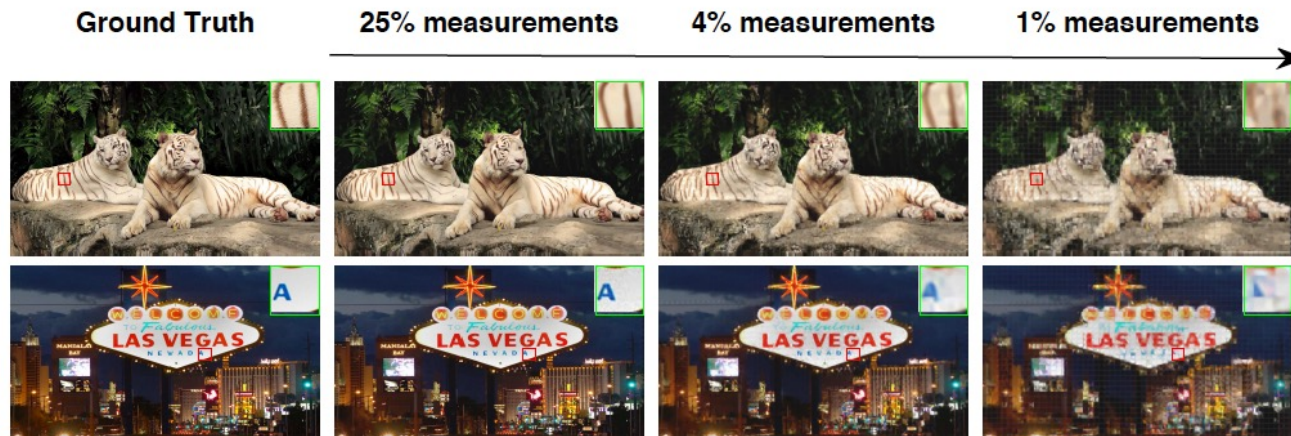


Figure 6: Compressive imager testbed layout with the object imaging arm in the center, the two DMD imaging arms are on the sides.

Standard compressive sensing problem:

$$\min_{\mathbf{x}} \|\Psi \mathbf{x}\|_1 \quad s.t \quad \|\mathbf{y} - \Phi \mathbf{x}\|_2 \leq \epsilon.$$

Use iterative solvers to determine \mathbf{x}

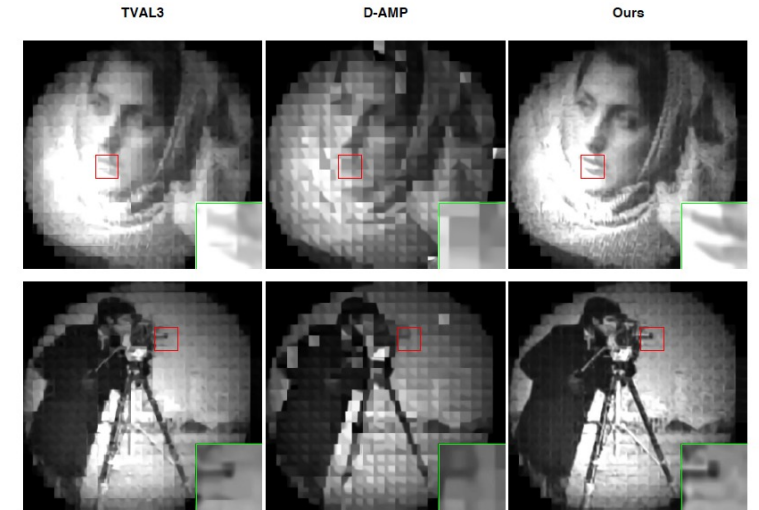
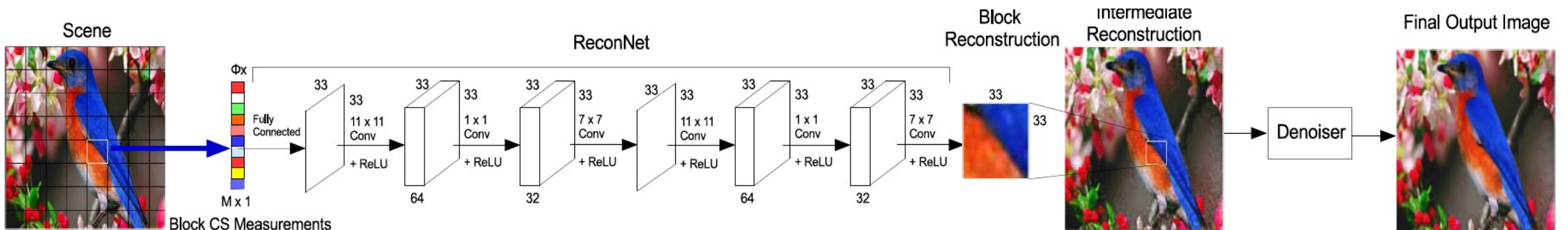


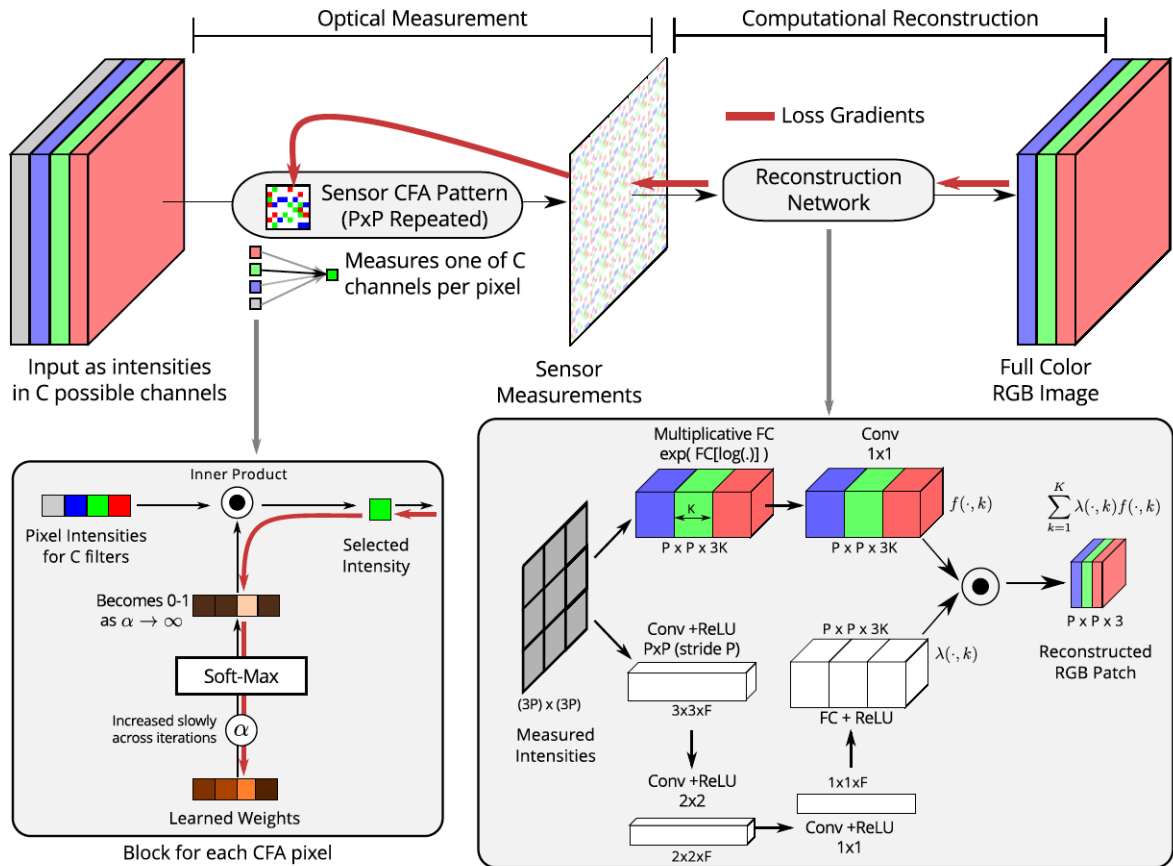
Figure 8: The figure shows reconstruction results on 3 images collected using our block SPC operating at measurement rate of 0.04. The reconstructions of our algorithm are qualitatively better than those of TVAL3 and D-AMP.

Proposed reconstruction method via CNN:



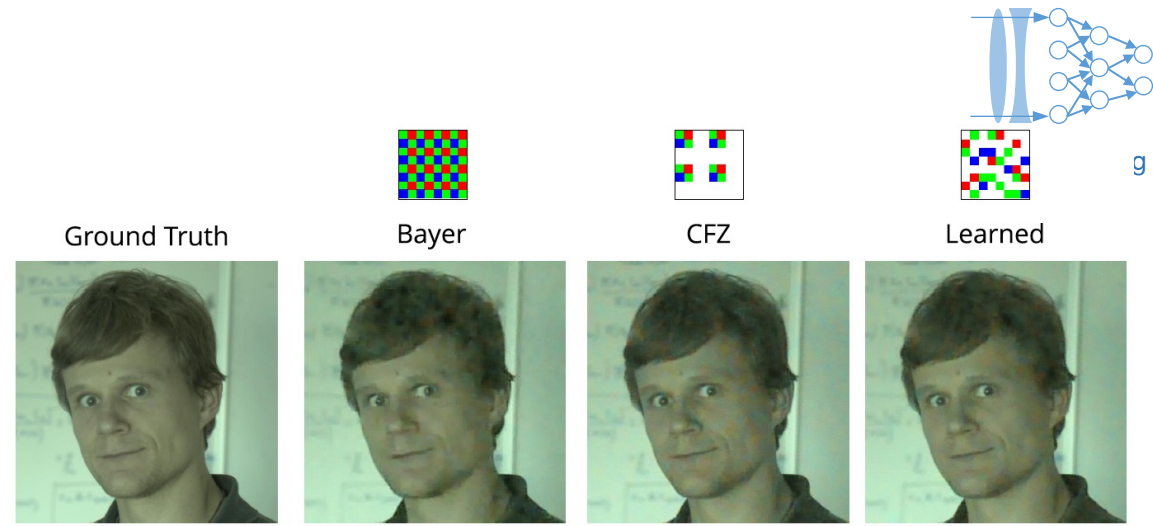
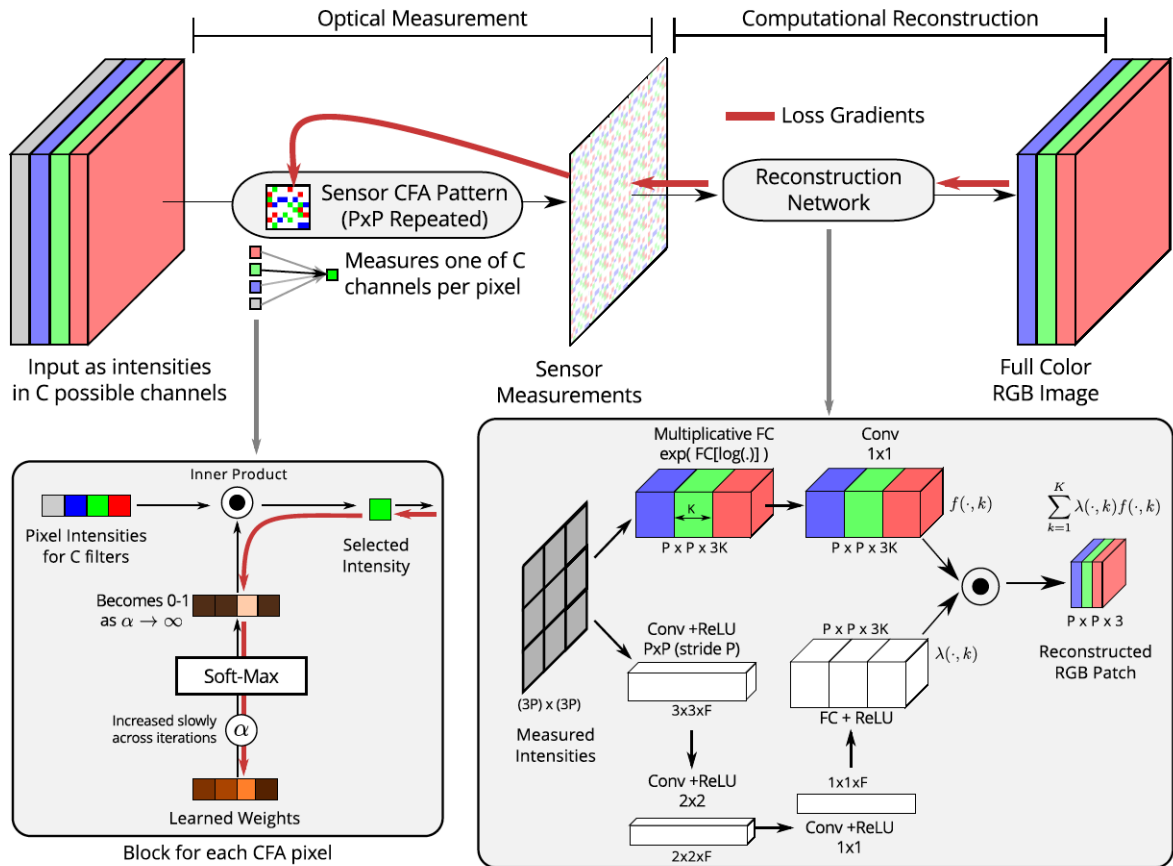
Learning Sensor Multiplexing Design through Back-propagation

Ayan Chakrabarti
 Toyota Technological Institute at Chicago
 6045 S. Kenwood Ave., Chicago, IL
 ayanc@ttic.edu



Learning Sensor Multiplexing Design through Back-propagation

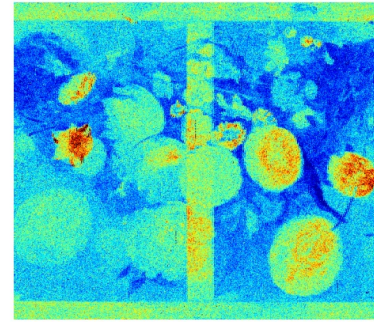
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Noise STD	Percentile	Bayer [2]	CFZ [4]	Learned
0	25%	47.62	48.04	47.97
	50%	51.72	52.17	52.12
	75%	54.97	55.32	55.30
0.0025	25%	44.61	46.05	46.08
	50%	47.55	49.08	49.17
	75%	50.52	51.57	51.76
0.0050	25%	42.55	44.33	44.37
	50%	45.63	47.01	47.19
	75%	48.73	49.68	49.94

Adaptive Image Sampling using Deep Learning and its Application on X-Ray Fluorescence Image Reconstruction

Qiqin Dai, Henry Chopp, Emeline Pouyet, Oliver Cossairt, Marc Walton, and Aggelos K. Katsaggelos, *Fellow, IEEE*

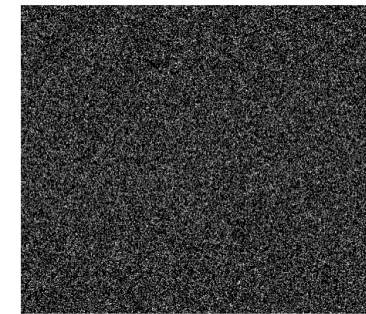
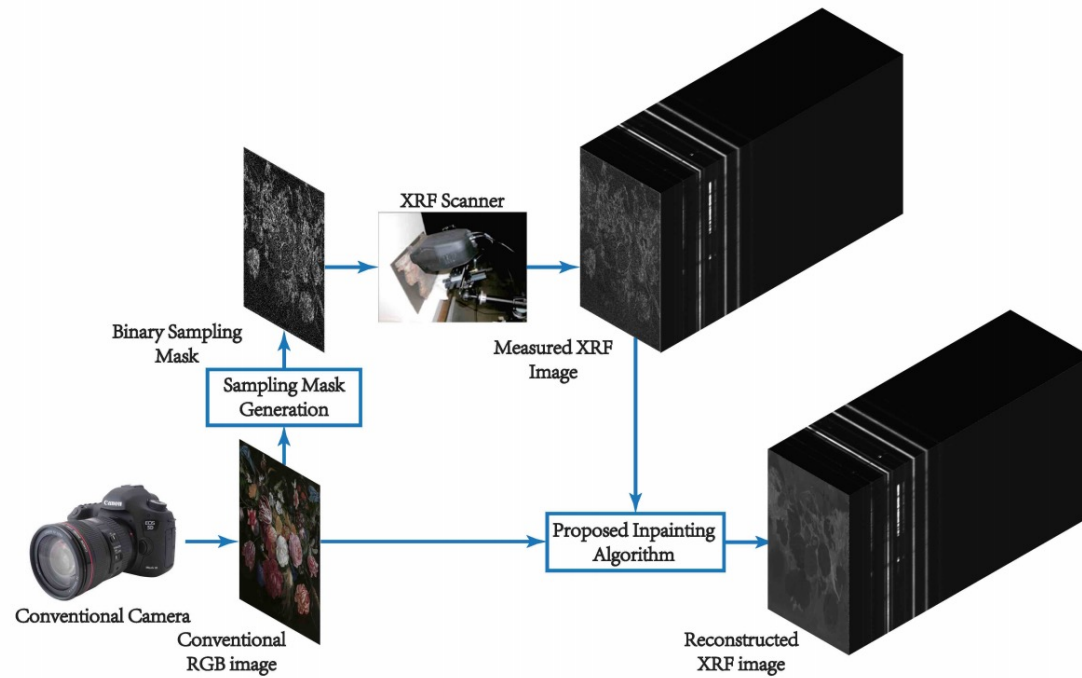


(a)

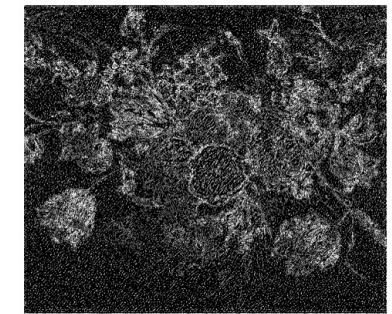


(b)

Fig. 1. (a) XRF map showing the distribution of $Pb L\eta$ XRF emission line (sum of channel #582 - 602) of the “Bloemen en insecten” (ca 1645), by Jan Davidsz. de Heem, in the collection of Koninklijk Museum voor Schone Kunsten (KMKSA) Antwerp and (b) the HR RGB image.

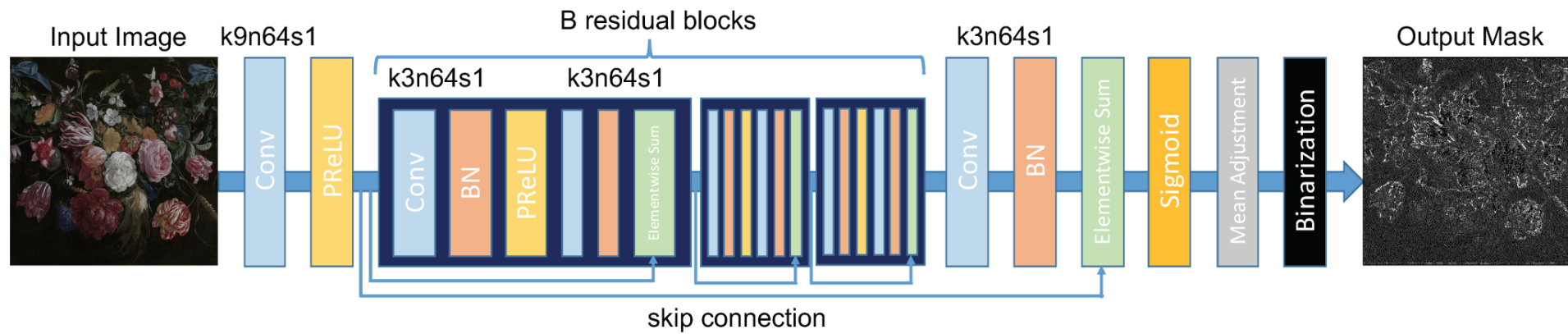
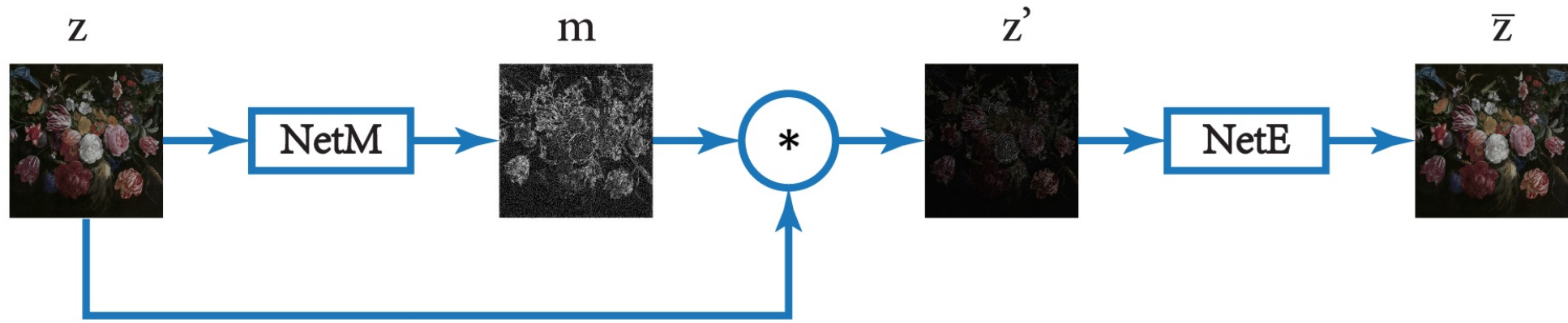


(a)



(b)

Fig. 2. (a) Random binary sampling mask that skips 80% of pixels and (b) Adaptive binary sampling mask that skips 80% of pixels based on the input RGB images in Fig 1 (b).



Learning a Variational Network for Reconstruction of Accelerated MRI Data

Kerstin Hammernik^{1*}, Teresa Klatzer¹, Erich Kobler¹,
Michael P Recht^{2,3}, Daniel K Sodickson^{2,3},
Thomas Pock^{1,4} and Florian Knoll^{2,3}

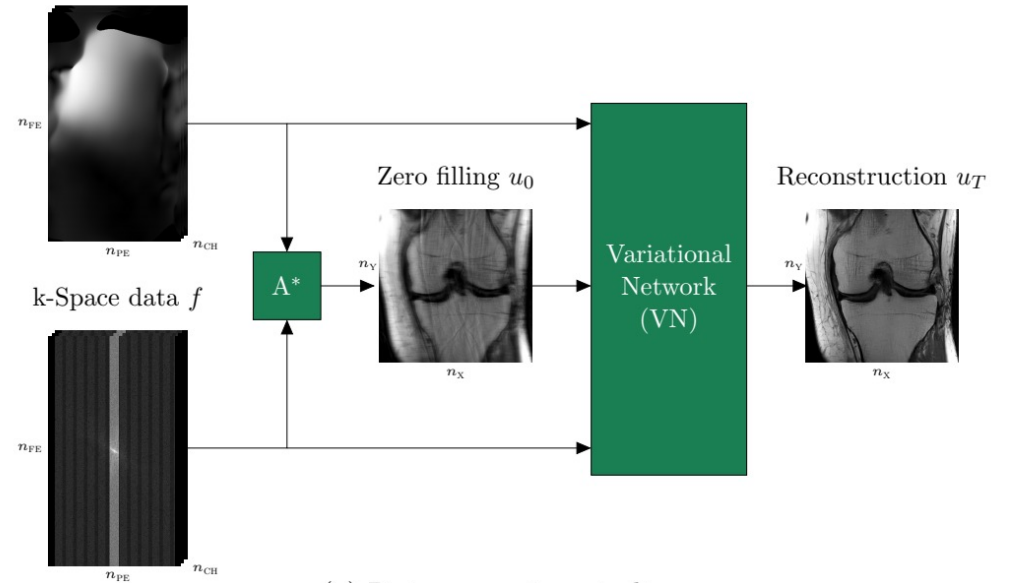
¹ Institute of Computer Graphics and Vision,
Graz University of Technology, Graz, Austria

² Center for Biomedical Imaging, Department of Radiology,
NYU School of Medicine, New York, NY, United States

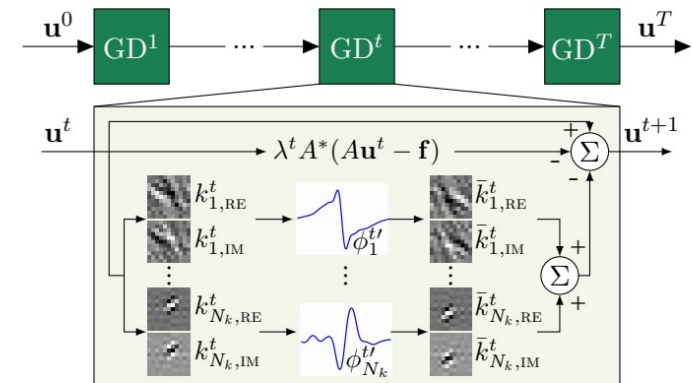
³ Center for Advanced Imaging Innovation and Research (CAI²R),
NYU School of Medicine, New York, NY, United States

⁴ Center for Vision, Automation & Control,
AIT Austrian Institute of Technology GmbH, Vienna, Austria

Sensitivity maps



(a) Data processing pipeline



(b) Structure of the variational network (VN)

Facebook Fast MRI Challenge:

<https://ai.facebook.com/blog/using-reinforcement-learning-to-personalize-ai-accelerated-mri-scans/>

Reducing Uncertainty in Undersampled MRI Reconstruction with Active Acquisition

Zizhao Zhang^{1,2,*} Adriana Romero² Matthew J. Muckley³ Pascal Vincent² Lin Yang¹ Michal Drozdal²
¹ University of Florida ² Facebook AI Research ³ NYU School of Medicine

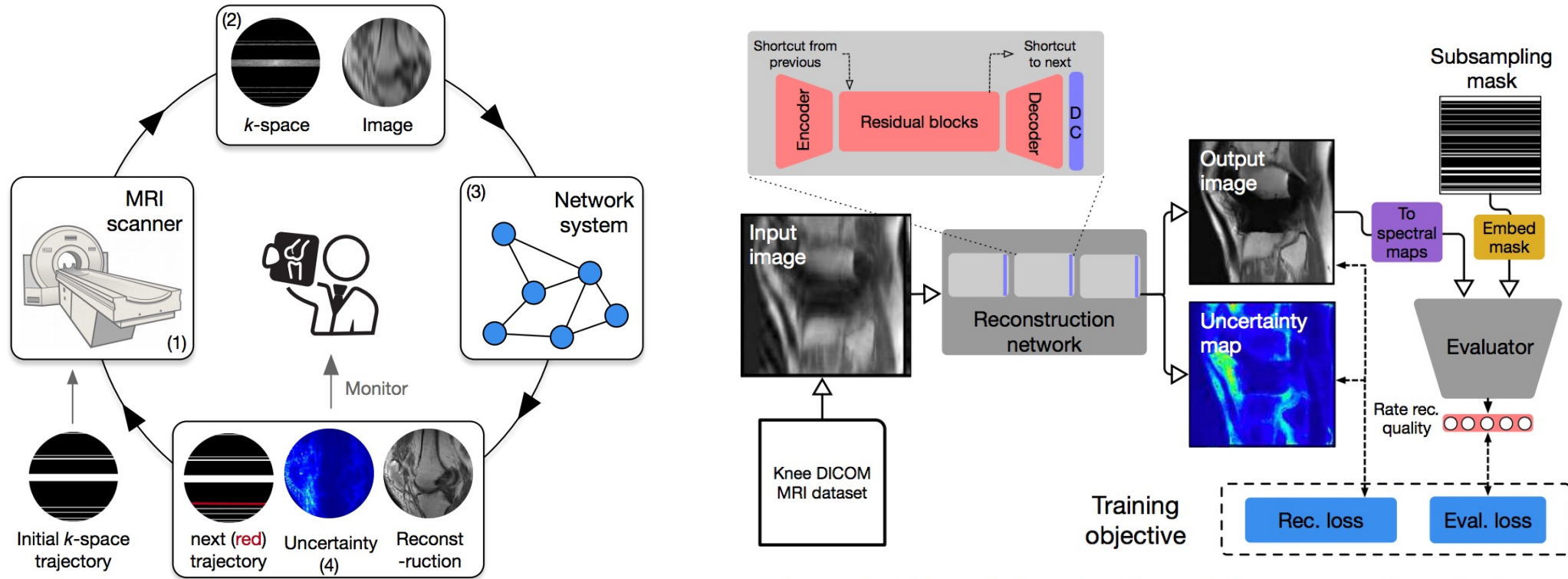


Figure 3: The training pipeline of the proposed method.

Learning a Probabilistic Strategy for Computational Imaging Sensor Selection

He Sun, *Member, IEEE*, and Adrian V. Dalca, *Member, IEEE*, and Katherine L. Bouman, *Member, IEEE*

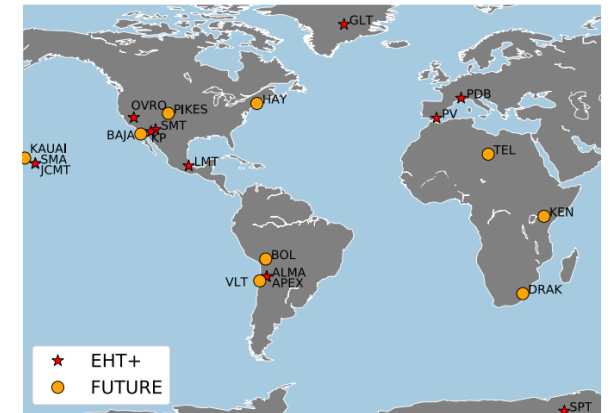
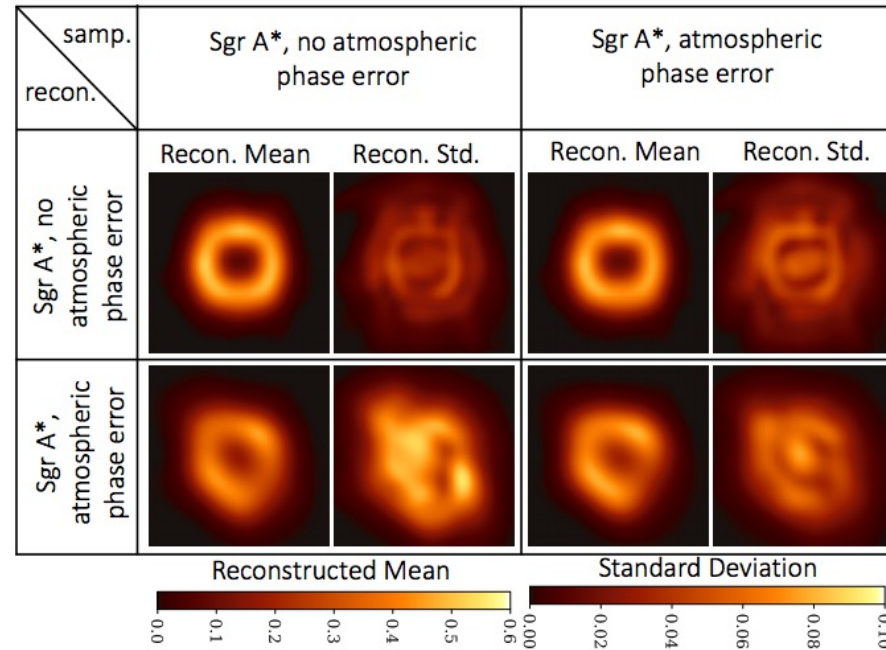
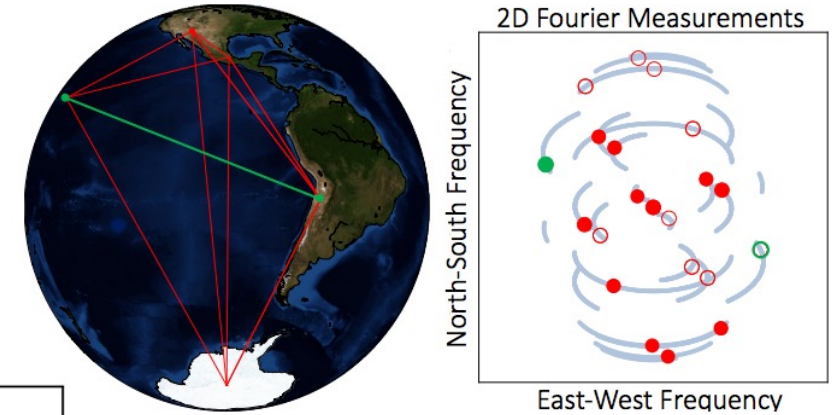
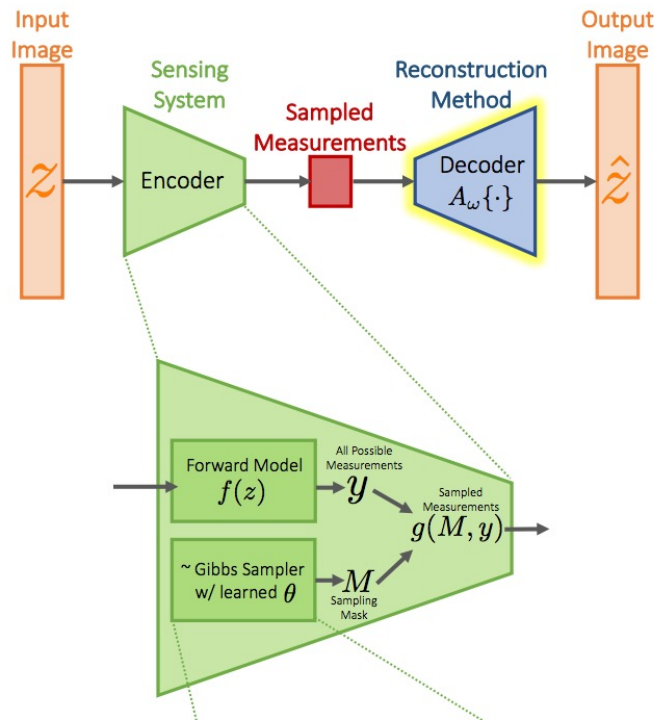


Fig. 3. Site map of potential future EHT telescope locations. Twelve sites (“EHT+”) marked with blue stars are existing telescopes currently participating in or planning to join the EHT. The other nine sites (“FUTURE”), marked with orange dots, are potential locations where new telescopes could be added. “FUTURE” sites are selected as locations that can observe at the necessary 230 GHz (1.3 mm wavelength) observed by the EHT.

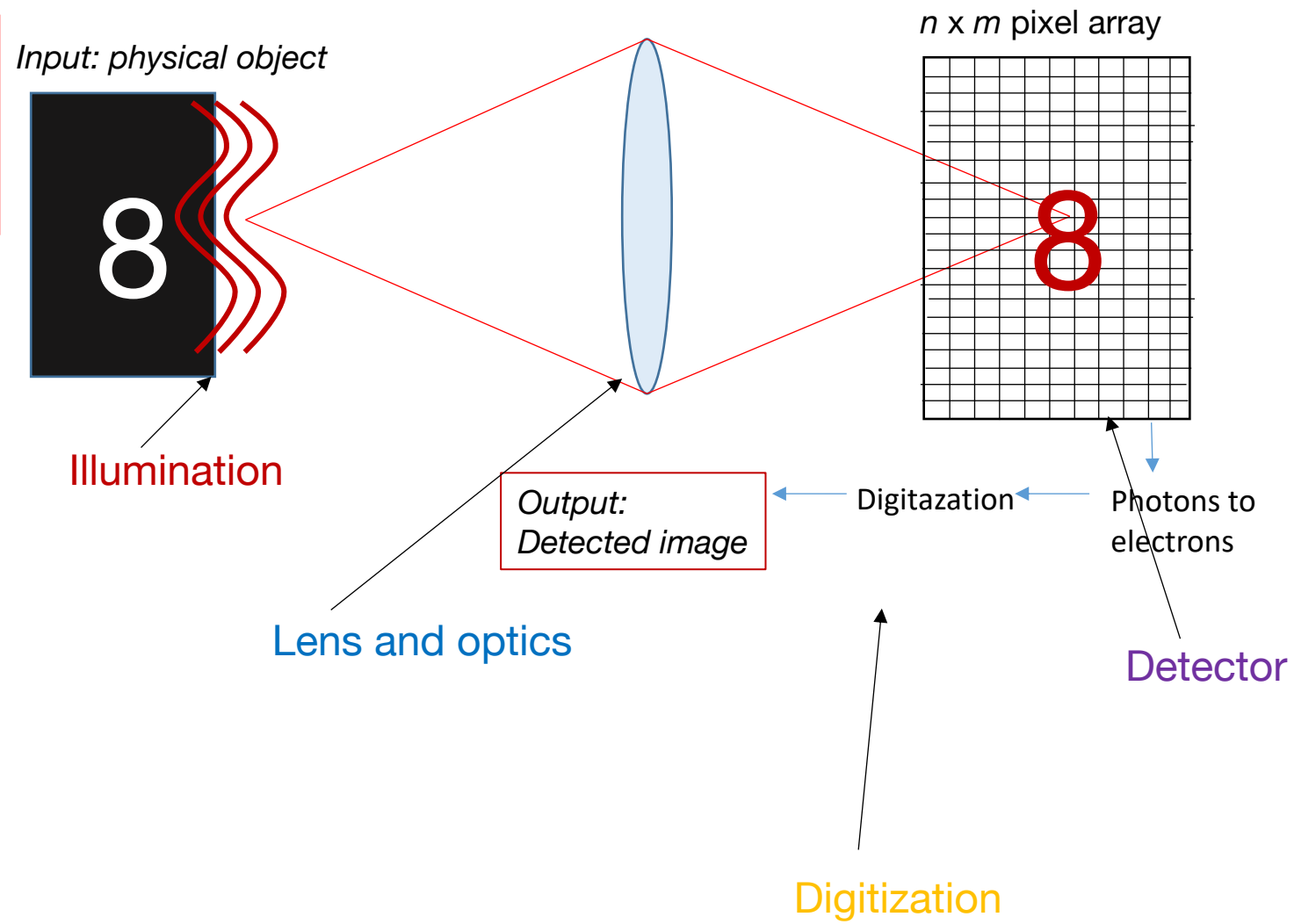
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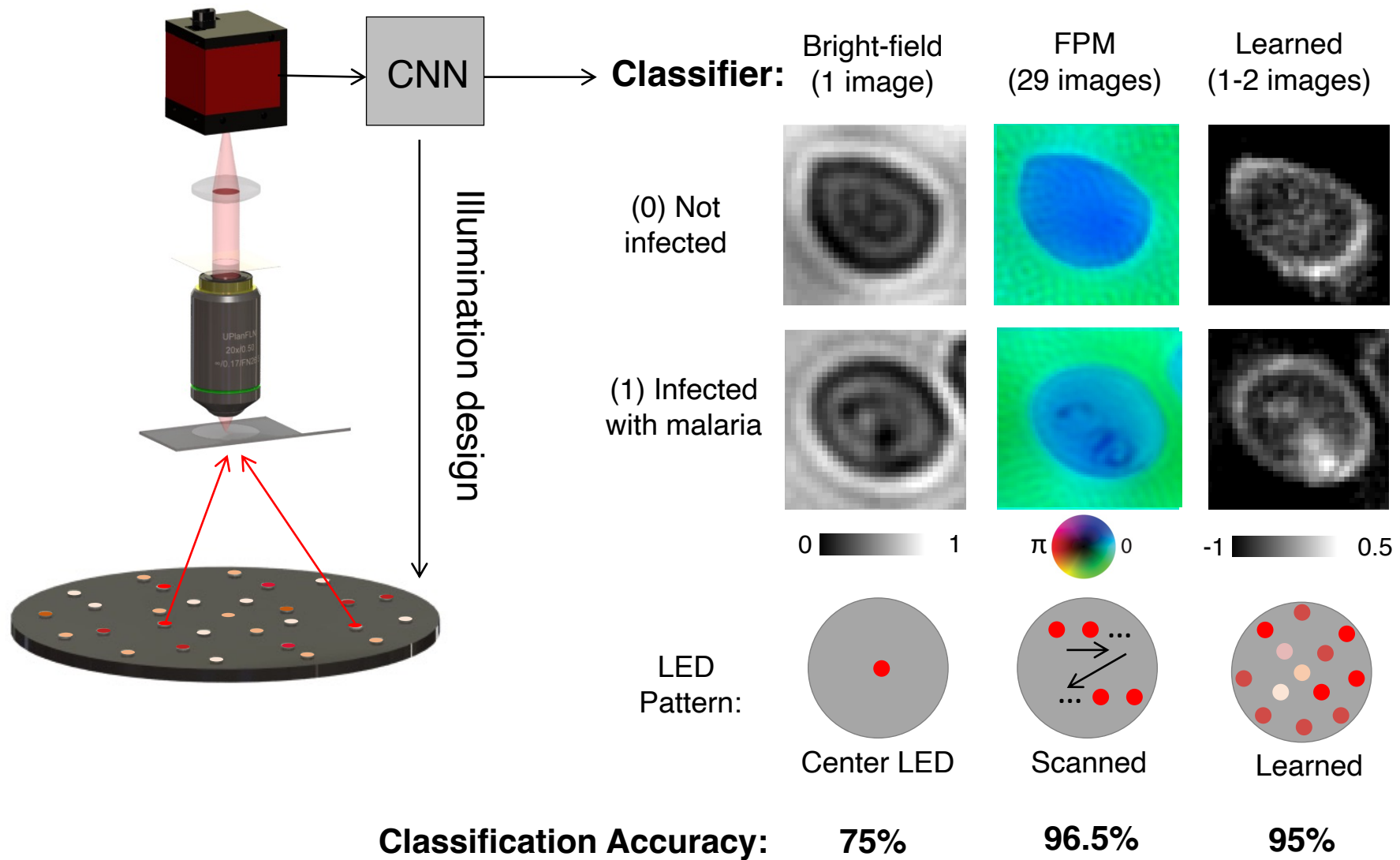
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Examples: Illumination

Accurate and efficient classification with LED illumination



R. Horstmeyer et al., "Convolutional neural networks that teach microscopes how to image," arXiv (2017)

Physics-based Learned Design: Optimized Coded-Illumination for Quantitative Phase Imaging

Michael R. Kellman^{*,§} Emrah Bostan^{*} Nicole Repina[‡]
 Michael Lustig^{*} Laura Waller^{*}

August 13, 2018

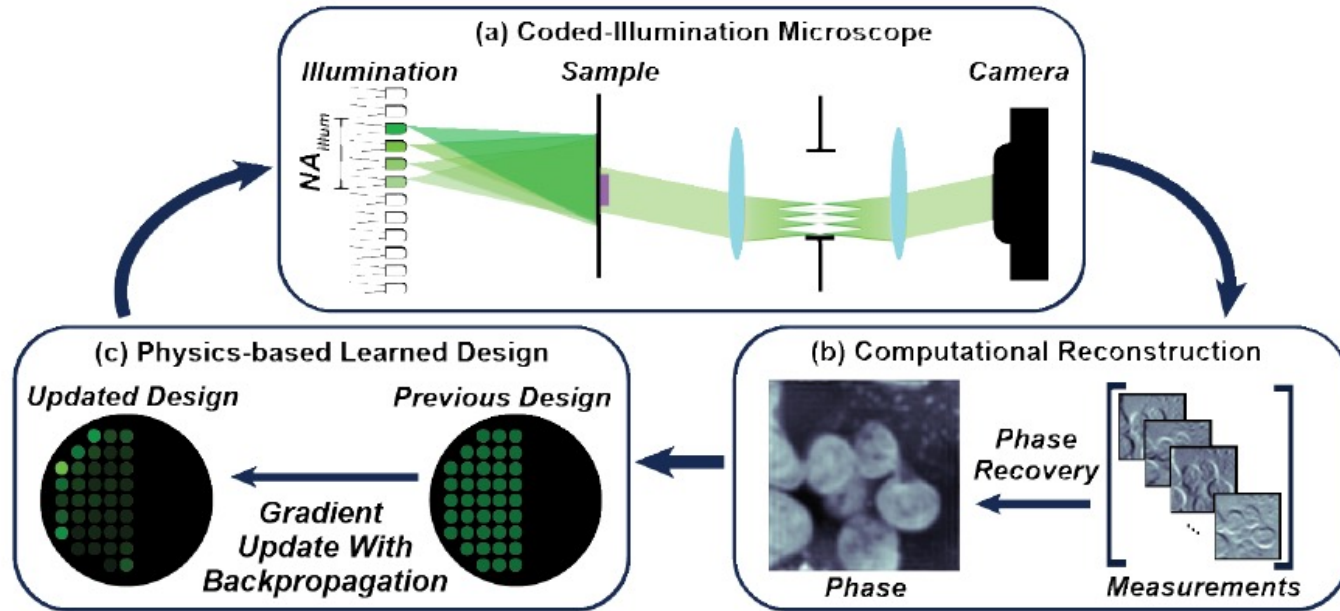
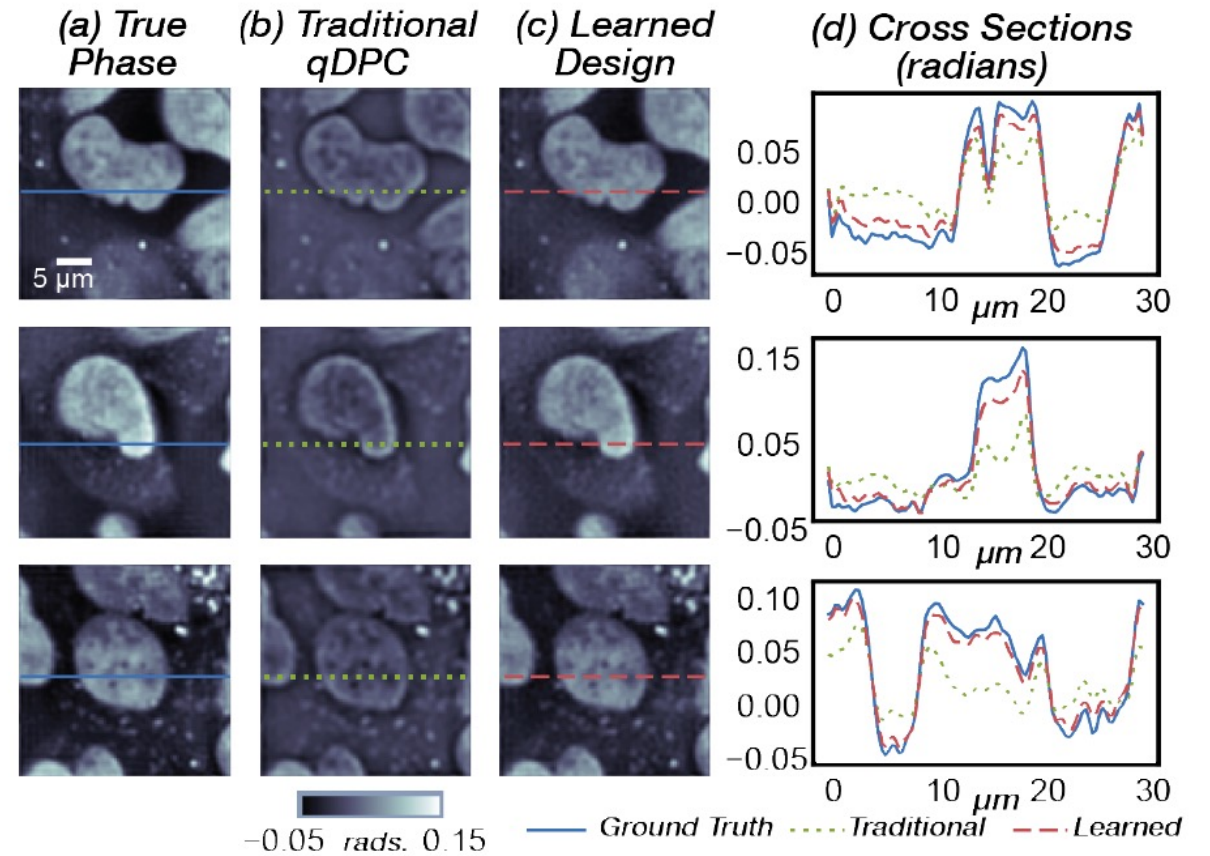
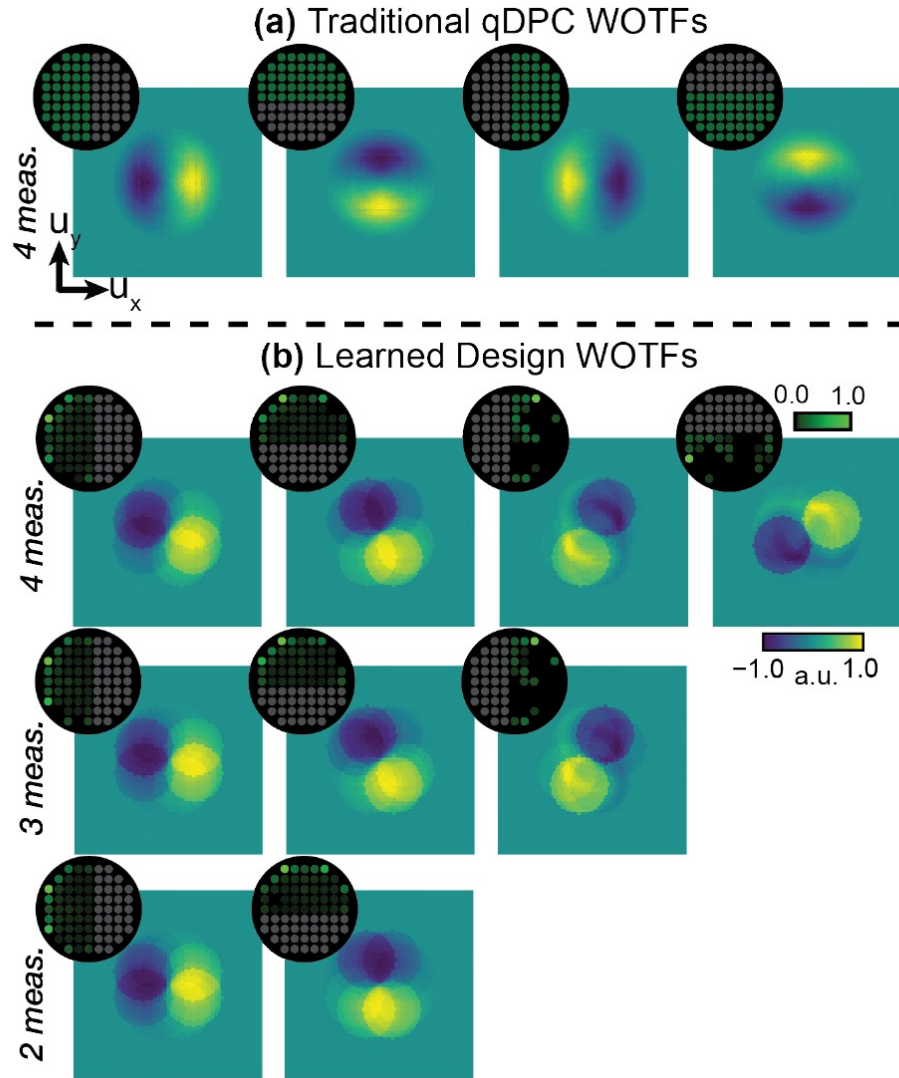
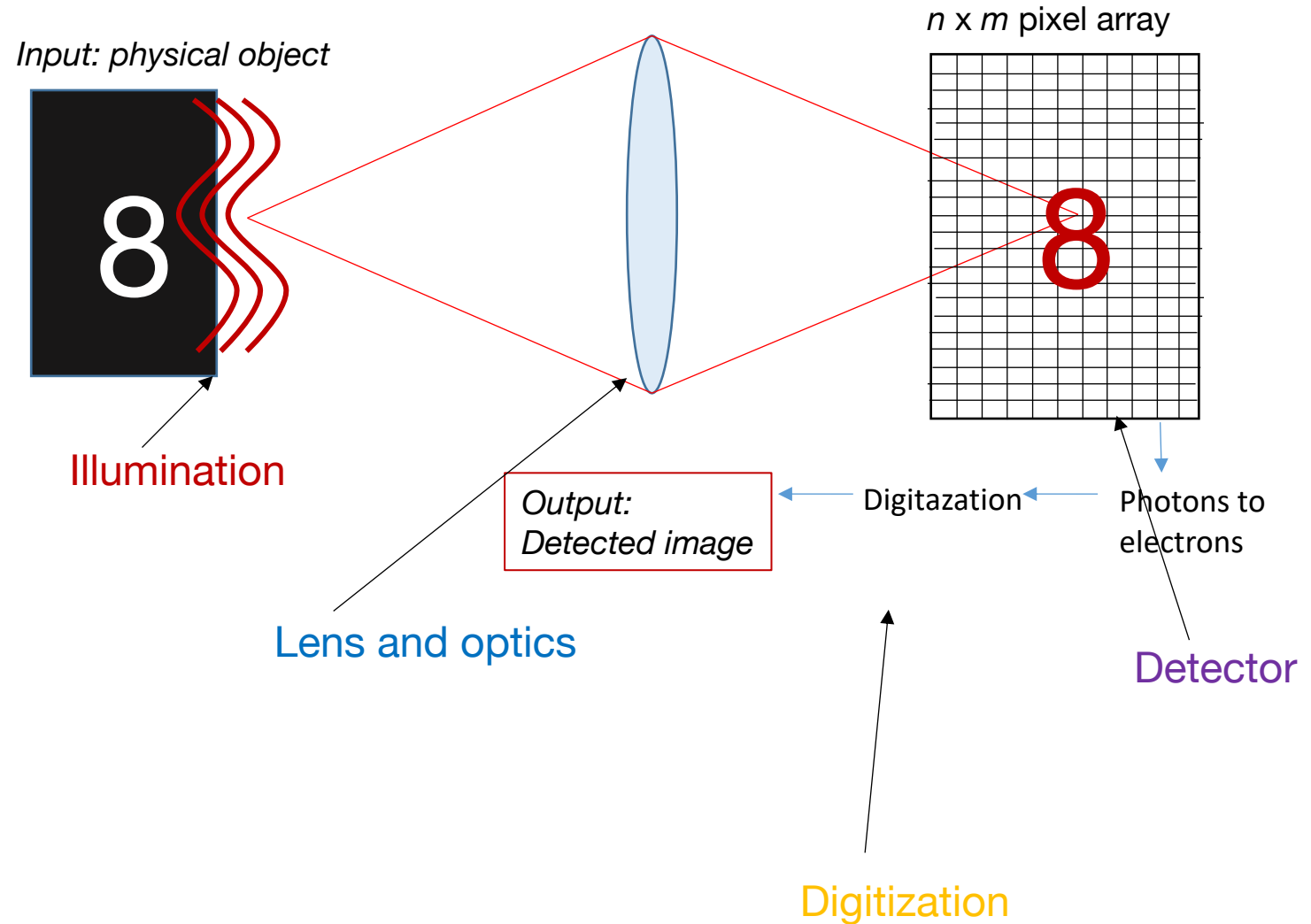


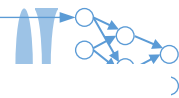
Figure 1: Learning Coded-Illumination Design for Quantitative Phase Imaging: (a) Schematic of the LED-illumination microscope where multiple intensity measurements are captured under unique coded-illumination patterns, (b) Computational phase reconstruction of the sample's optical phase with coded-illumination measurements. (c) Optimization for learning of coded-illumination design based on the non-linear iterative reconstruction.



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 - Pixel shape & fill factor
 - Color filters
 - Other filters
- **Digitization**
 - E to P curves
 - Digitization schemes/thresholds
 - Data transmission, multiplexing
- Physical objects





Deep learning with coherent nanophotonic circuits

Yichen Shen , Nicholas C. Harris , Scott Skirlo, Mihika Prabhu, Tom Baehr-Jones, Hochberg, Xin Sun, Shijie Zhao, Hugo Larochelle, Dirk Englund & Marin Soljačić


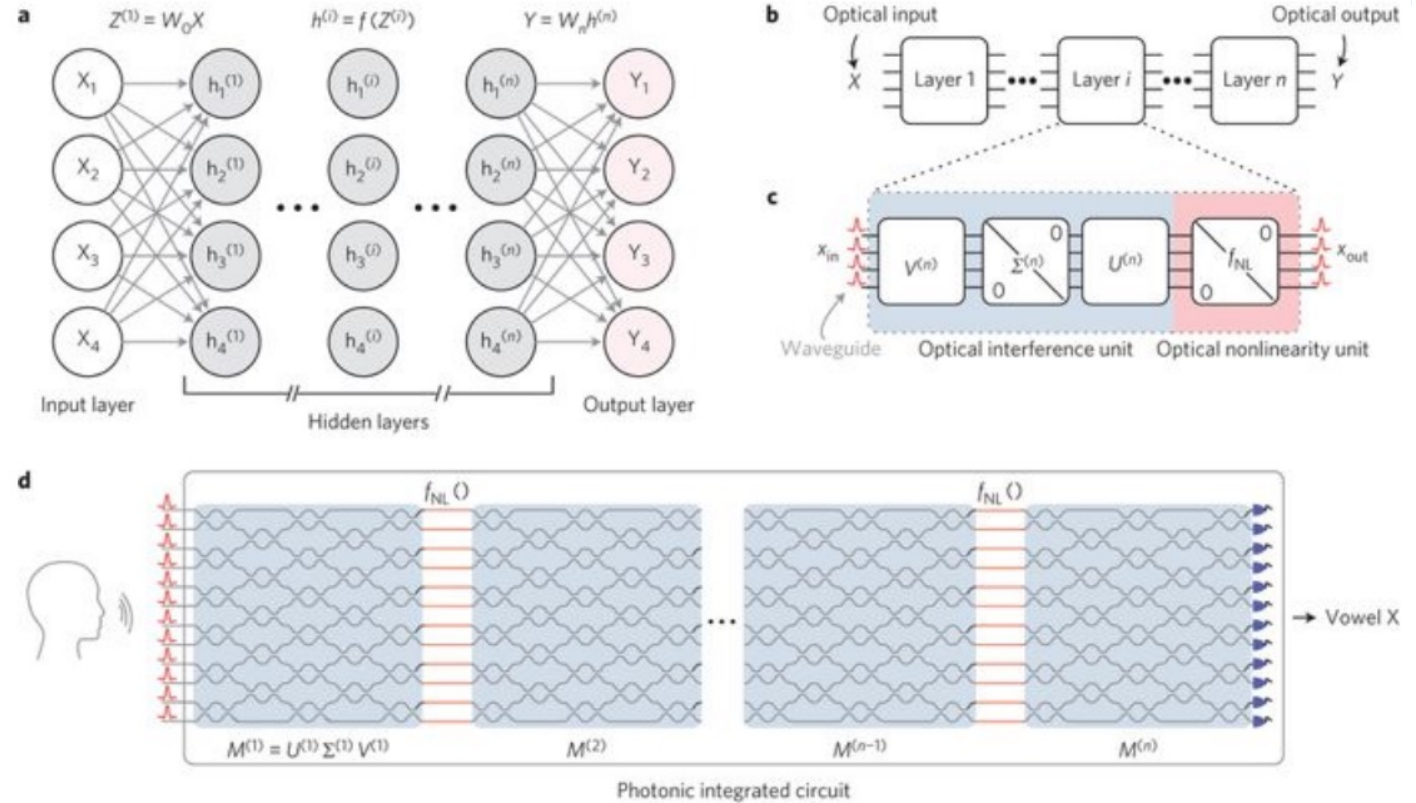
Nature Photonics **11**, 441–446 (2017) | [Download Citation](#) 

Figure 1: General architecture of the ONN.



a, General artificial neural network architecture composed of an input layer, a number of hidden layers and an output layer. **b**, Decomposition of the general neural network into individual layers. **c**, Optical interference and nonlinearity units that compose each layer of the artificial neural network. **d**, Proposal for an all-optical, fully integrated neural network.

Figure 2: Illustration of OIU.

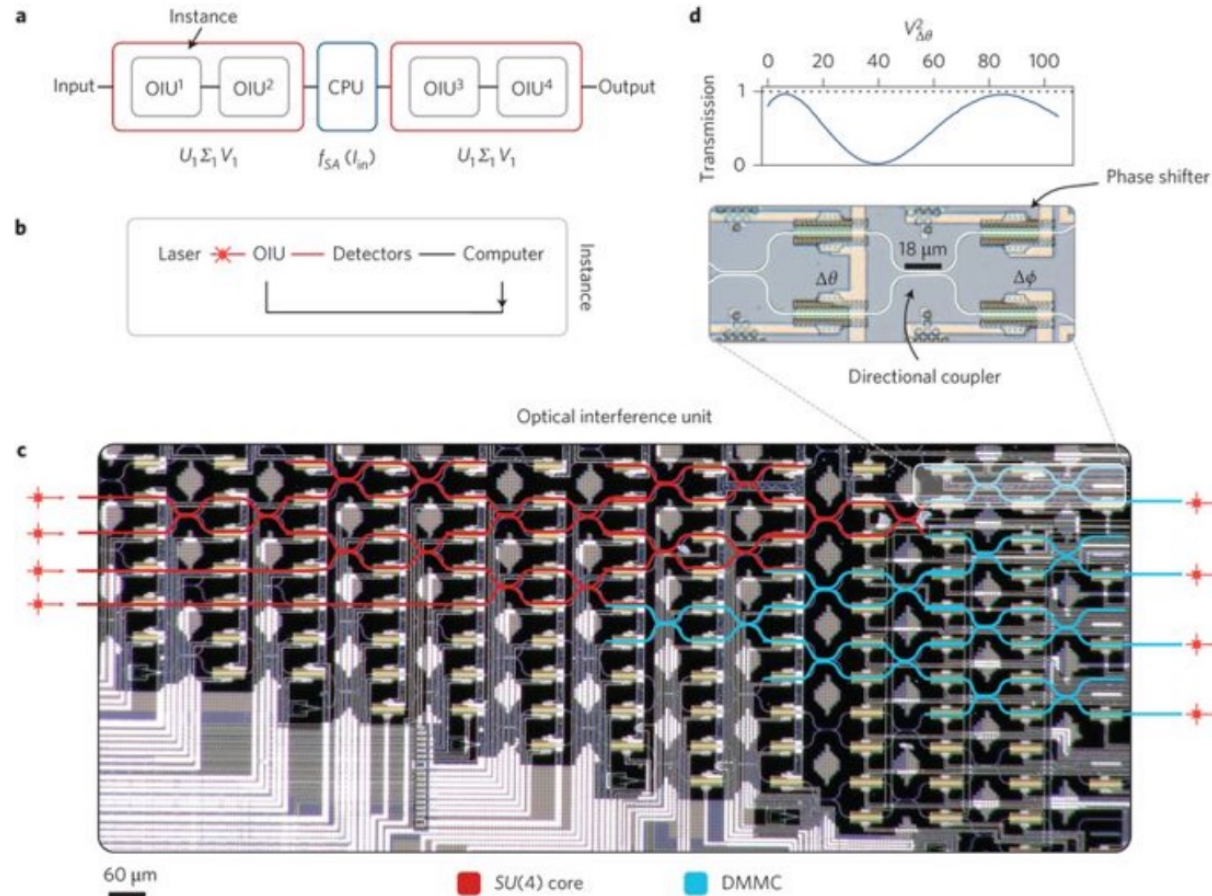
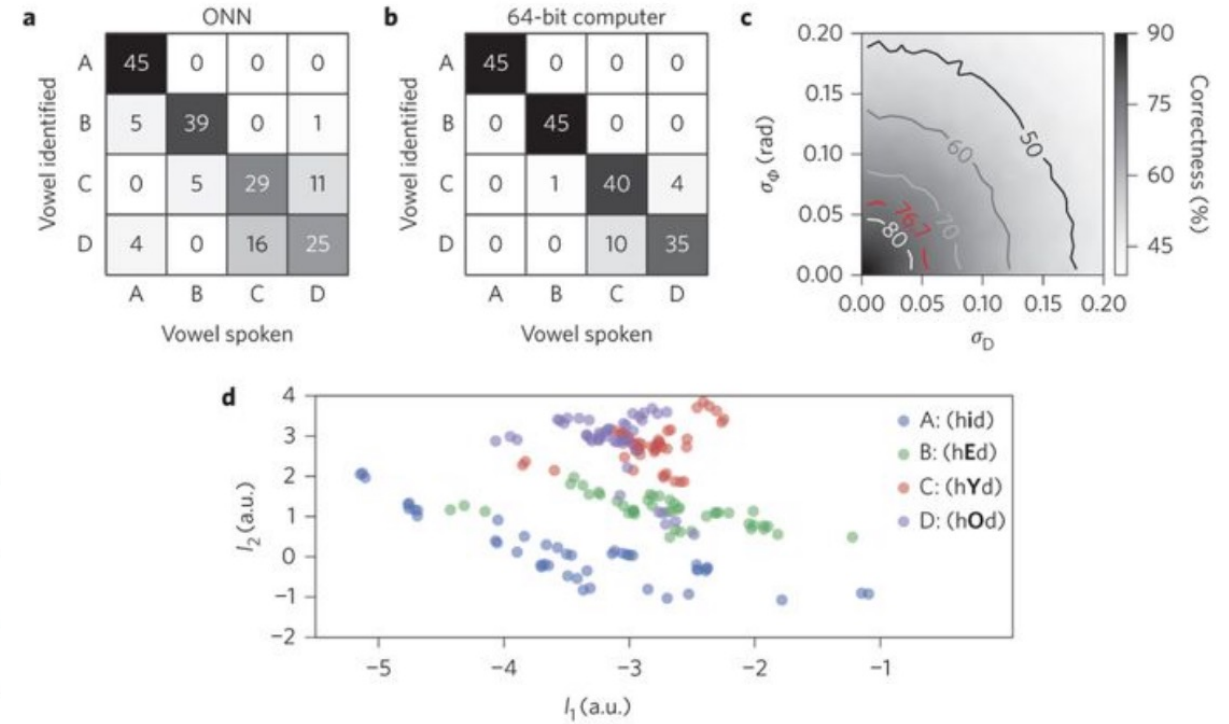
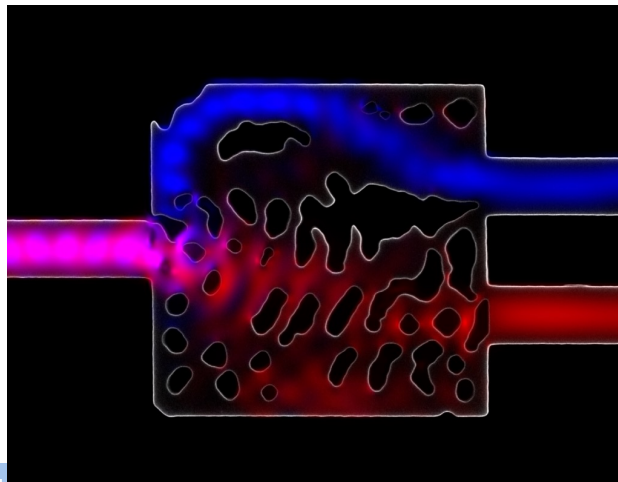
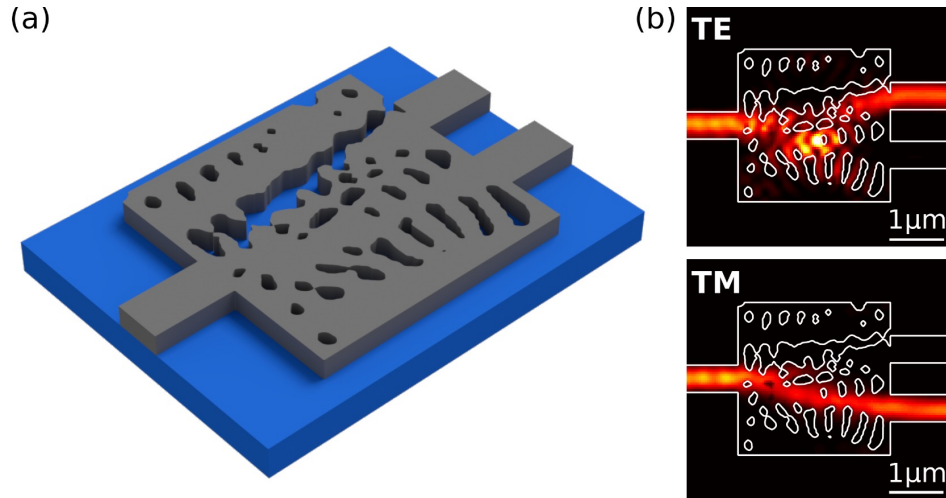


Figure 3: Vowel recognition.



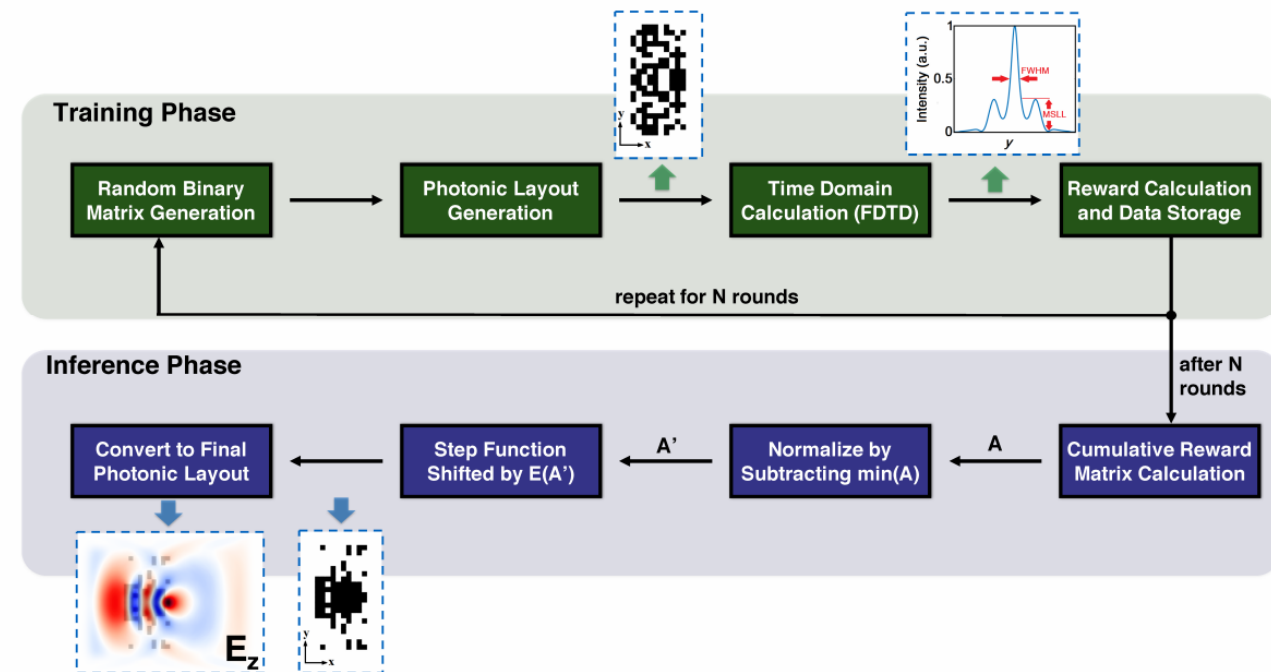
Inverse design in nanophotonics

Sean Molesky¹, Zin Lin², Alexander Y. Piggott³, Weiliang Jin¹, Jelena Vucković³ and Alejandro W. Rodriguez^{1*}



Machine learning based compact photonic structure design for strong light confinement

MIRBEK TURDUEV^{1,5,*}, CAGRI LATIFOGLU^{2,5}, IBRAHIM HALIL GIDEN^{3,6}, and Y. SINAN HANAY^{4,5}



Ethical questions surrounding deep convolutional networks

1. What are your expectations for an image reconstruction algorithm used in a clinical setting?

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Ethical questions surrounding deep convolutional networks

1. What are your expectations for an image reconstruction algorithm used in a clinical setting?
2. What types of “guarantees” should we be able to make, if any, to a patient?
3. How should we guide future development of ML software to meet any guarantees?
4. How should we guide future development of ML-designed hardware to meet any guarantees?
5. Thoughts towards a system of checks and balances?

The Machine Learning in Imaging Ethics Questionnaire

Situation 1: In 5 years, you walk into a clinic because you have a spot on your skin that you are concerned about. The clinician is too busy, so you step over to a terminal with a standard microscope and it images your arm. It says you are fine.

Are you comfortable with leaving the office?

Yes:

No:

Why or why not? What might change how you feel?

The Machine Learning in Imaging Ethics Questionnaire

Situation 2: The same thing happens. But this time, the machine reports that it is 99% confident in its diagnosis, given previous examples of skin marks that have been verified by doctors as benign. It also gives you the opportunity to take a look at some of these previous example images it is basing its decision on. You notice that they don't look 100% like the mark on your arm, as is expected, but they look pretty similar.

Are you comfortable with leaving the office?

Yes:

No:

Why or why not? What might change how you feel?

The Machine Learning in Imaging Ethics Questionnaire

Situation 3: In 5 years, the same thing happens. But this time, a doctor comes up after the machine makes its suggested diagnosis. He takes a very cursory look (10 seconds) and then confirms the machine's opinion.

Are you now comfortable with leaving the office?

Yes:

No:

The Machine Learning in Imaging Ethics Questionnaire

Situation 4: In 10 years, you go up to a modified microscope, “the Tissue Scanner 3000”, that has a number of fancy lenses and lights. As a machine learning expert by now, you’re aware that this microscope is optimized for looking at skin lesions. It performs a scan with a particular lighting configuration and reports a score of 98% confident that the lesion is benign, allowing you to look through other examples. It asks if you’d like another scan for additional confidence or a different outcome, at which point the illumination changes and it does some more scanning and reports a 99% confidence level. You can continue with another scan, but...

Are you now comfortable with leaving the office?

Yes:

No: